



**REVIEW**

# A Review of the Application of Artificial Intelligence in Orthopedic Diseases

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## ABSTRACT

In recent years, Artificial Intelligence (AI) has revolutionized people's lives. AI has long made breakthrough progress in the field of surgery. However, the research on the application of AI in orthopedics is still in the exploratory stage. The paper first introduces the background of AI and orthopedic diseases, addresses the shortcomings of traditional methods in the detection of fractures and orthopedic diseases, draws out the advantages of deep learning and machine learning in image detection, and reviews the latest results of deep learning and machine learning applied to orthopedic image detection in recent years, describing the contributions, strengths and weaknesses, and the direction of the future improvements that can be made in each study. Next, the paper also introduces the difficulties of traditional orthopedic surgery and the roles played by AI in preoperative, intraoperative, and postoperative orthopedic surgery, scientifically discussing the advantages and prospects of AI in orthopedic surgery. Finally, the article discusses the limitations of current research and technology in clinical applications, proposes solutions to the problems, and summarizes and outlines possible future research directions. The main objective of this review is to inform future research and development of AI in orthopedics.

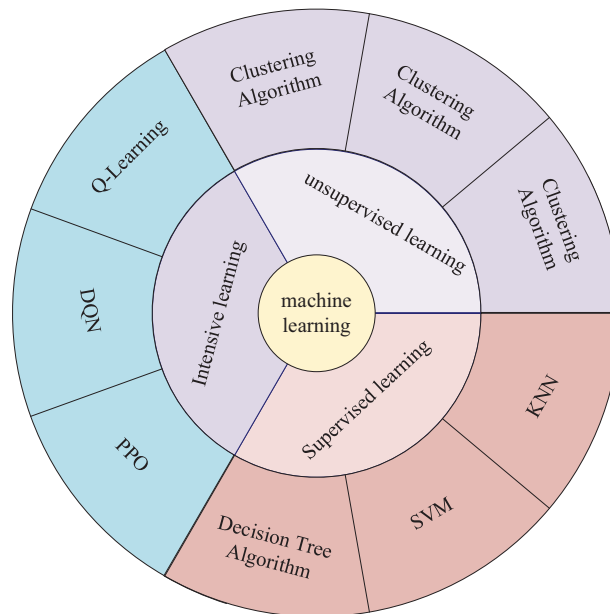
## KEYWORDS

Artificial intelligence; orthopedics; image detection; deep learning; machine learning; diagnostic disease; robotics

## 1 Introduction

Artificial Intelligence (AI) has been closely connected with human life in recent years, and people are affected by AI everywhere. The concept of AI was first proposed by Prof. John McCarthy in 1956. It involves “the science and engineering of making intelligent machines, outstanding computer programs” [1]. AI is a technology that enables computers, computer-controlled robots, or software to think like humans. AI utilizes research results to develop intelligent software and systems by studying how the human brain thinks and how humans solve problems, learn, make decisions, and work. AI has many branches, with this study focusing specifically on Machine Learning (ML). While other branches of AI have significantly impacted science and technology, machine learning is undoubtedly the most researched direction in medical research applications today. ML allows machines to automatically learn and improve from experience without requiring human programming to specify rules and logic. Fig. 1 shows the components and primary models of machine learning. ML usually requires manual extraction of features, a process known as feature engineering.

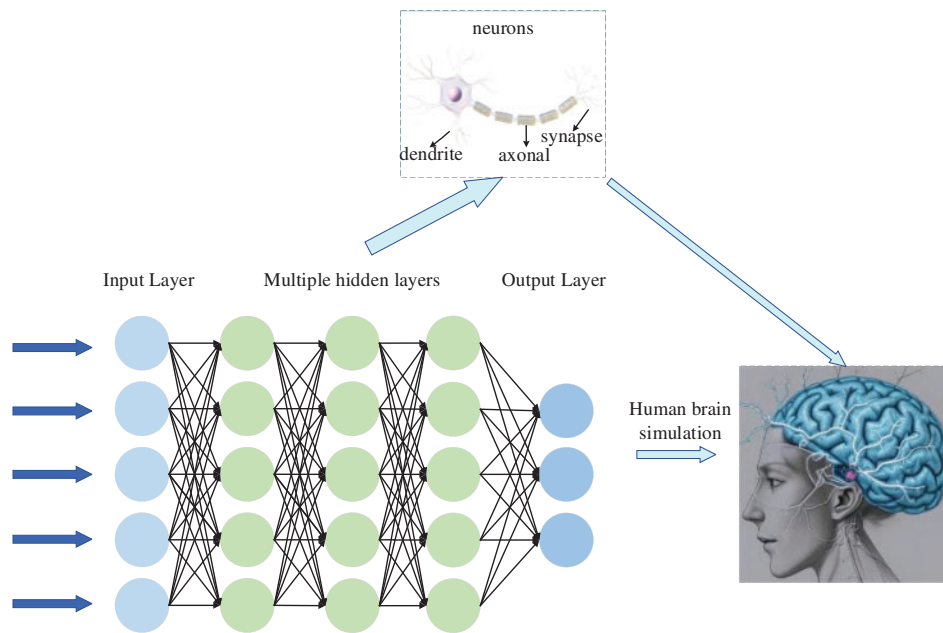




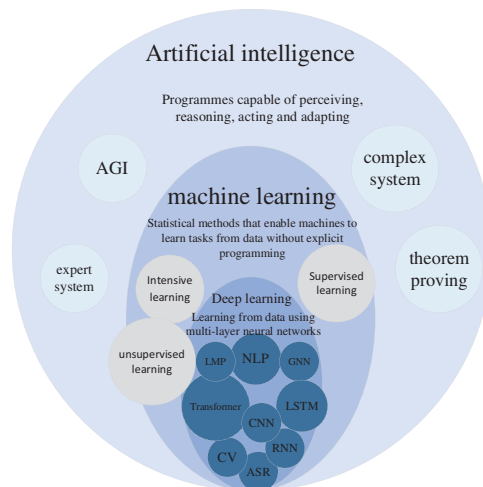
**Figure 1:** Components and main models of machine learning

In most cases, feature engineering can be done efficiently; however, it is very challenging to be helpful in image detection. We want machines to automatically learn features from image data, thus reducing human workload. McCulloch et al. [2] were inspired by biology. They proposed a one-of-a-kind network similar to a biological neural network, miming its structure, implementation mechanism, and function. A network of artificial neurons typically consists of several layers containing an input layer, one or more hidden layers, and an output layer. In the hidden layers, researchers can refine the training by adjusting the neural network's structure and the neuron nodes' weights. Artificial Neural Networks (ANNs) allow computational models with multiple processing layers to learn multiple levels of abstract data representation. With the backpropagation algorithm, the model can indicate how to change the internal structure to find complex structures in large datasets. The principle of Artificial Neural Network (ANN) is shown in Fig. 2. Deep learning is a branch of machine learning that centers on ANNs. Deep Learning (DL) is far more effective than previous related techniques in speech and image recognition [3]. Unlike general ML, DL automatically learns high-dimensional abstractions of data through neural networks, reducing the composition of feature engineering and placing more emphasis on model structure, nonlinear processing, feature extraction, and feature transformation. The relationship between AI, ML, and DL is shown in Fig. 3.

At this stage, as medical data metrics continue to grow and the volume of data increases dramatically, there is an urgent need for robust data processing capabilities to support the medical field. Today, medical imaging is growing at an annual rate of up to 30%. While the demand for medical imaging is slowing down, it is still much higher than the 1.8% annual growth rate for radiologists. The growth in medical imaging demand far exceeds the physicians' supply [4]. Today's AI is integrated into people's daily healthcare with investments of over \$1.5 billion and growing [5]. The application of AI in medical imaging can help doctors make quick and accurate diagnoses and develop the proper medical treatment plan, which meets the current needs and has considerable potential in the coming years.



**Figure 2:** Deep neural network



**Figure 3:** Relationship between artificial intelligence, machine learning and deep learning

The field of orthopedics encompasses a wide range of conditions such as joint replacement, spinal correction, traumatic orthopedics, cartilage, and osteoarthritis, all of which require rigorous patient planning, including patient characterization, preoperative evaluation, intraoperative assistance, and postoperative rehabilitation. Personalized treatment can significantly improve diagnostic and surgical accuracy and medical efficiency. In medical fields such as radiology, dermatology, and cardiology, AI has already succeeded, surpassing senior experts in some areas. Cabitza et al. [6] report a 10-fold increase in machine-learning-related articles in the orthopedic literature since 2010. However, by deeply analyzing the relevant literature in this field in recent years, we found that applying relevant research in orthopedics to the clinic is still very challenging, and the application of AI in orthopedics

is still in the developmental stage [7]. Although OsteoDetect, an AI based on deep learning, has been approved by the U.S. Food and Drug Administration (FDA) in 2018 for the detection and assisted diagnosis of wrist fractures in adults and has achieved good results, it is still deficient in penetration and clinical application. Therefore, applying AI to orthopedic diseases is still a pressing issue for current researchers. The purpose of this review is to provide an understanding of the concept of AI based on the analysis of a large number of studies in the field of orthopedics, to summarize the recent studies of AI in orthopedics in the last few years with the related improved methods, and to analyze the current limitations and the future development direction.

## 2 Advances in the Application of Artificial Intelligence to Orthopedic Image Detection

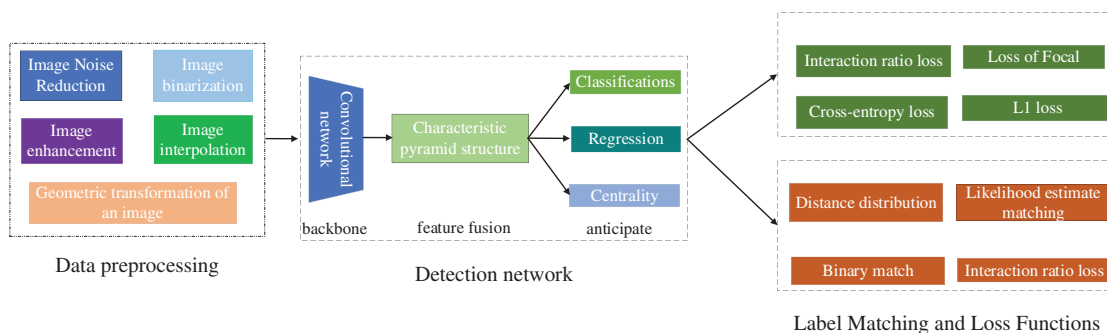
The diagnosis of many orthopedic diseases often relies on image judgment. However, there are many types of orthopedic diseases, and the similarity of different diseases is exceptionally high, which often causes young physicians to misdiagnose. Missed diagnosis in determining a patient's illness will not only waste medical resources but also affect further patient treatment and aggravate the deterioration of the patient's condition.

DL image processing techniques are categorized into image classification, target recognition, and semantic segmentation. Image classification techniques are mainly used to distinguish disease categories, while target recognition and semantic segmentation are used for lesion detection. Introducing deep learning into medical image detection, utilizing its powerful learning ability and excellent image segmentation ability, makes up for the shortcomings of traditional medical image recognition, such as slow speed and poor recognition effect, that makes the medical image obtain essential information and realizes more accurate classification, recognition and segmentation [8].

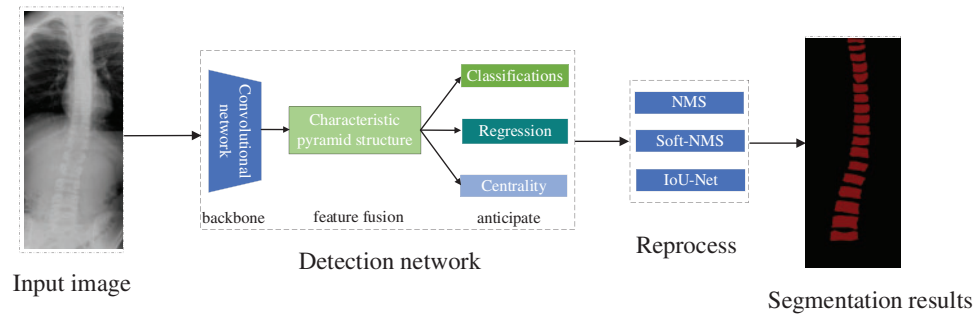
### 2.1 Deep Learning Orthopedic Image Detection Fundamentals

#### 2.1.1 Deep Learning Orthopedic Image Detection Process

Orthopedic image detection based on deep learning consists of two main parts: training aims to use the training set for parameter learning of the detection network, and the process of the training phase mainly includes data preprocessing, detection network, and label matching and loss calculation, and finally generates data such as evaluation indexes. Testing aims to detect the model's generalization ability, which determines whether the model can be used in the clinic. The testing phase mainly consists of input images, detection network, post-processing, and finally, the generated detection results. The deep learning image detection training process is shown in Fig. 4. The scoliosis image and detection results are shown in Fig. 5.



**Figure 4:** Deep learning image detection training process



**Figure 5:** Spinal curvature image testing process and results

2.1.2 Model Evaluation Metrics

Table 1 lists the commonly used evaluation metrics for image detection. The metrics can most intuitively reflect the model’s performance and the direction of future improvement.

**Table 1:** Image detection evaluation index

Indicator	Hidden meaning	Formula
Accuracy	Proportion of correctly predicted samples to total sample size.	$\text{Accuracy} = \frac{TP + TN}{TP + FP + TN + FN}$
Precision/(PPV)	Proportion of samples with positive predictions to all positive samples.	$\text{Precision} = \frac{TP}{TP + FP}$
Recall/Sensitivity	Number of correctly predicted samples as a percentage of the actual data set.	$\text{Recall} = \frac{TP}{TP + FN}$
Dice	Indicates the overlap similarity between the segmentation result and the markers. The value is between 0 and 1; the closer the range is to 1, the better the segmentation effect is.	$\text{Dice} = \frac{2TP}{FP + 2TP + FN}$
IOU	Describes the degree of overlap between two boxes; the more overlapping areas, the greater the value.	$\text{IOU} = \frac{\text{Area of Intersection of two boxes}}{\text{Area of Union of two boxes}}$
Specificity	The proportion of all negative cases predicted to be negative.	$\text{Specificity} = \frac{TN}{TN + FP}$
NPV	The proportion of samples categorized as negative that are negative.	$\text{NPV} = \frac{TN}{TN + FN}$
F1 Score	The F1 Score metric was introduced to weigh the conflicting metrics of Precision and Recall.	$\text{F1 Score} = \frac{2 * \text{Precision} * \text{Recall}}{\text{Precision} + \text{Recall}}$

(Continued)

**Table 1 (continued)**

Indicator	Hidden meaning	Formula
ROC (Receiver Operating Characteristic)	Used to assess whether the model generalization performance is good or bad. The larger the area under the line (AUC) of the ROC curve, the better the model generalization performance.	

The four indicators, True positives (TP), False positives (FP), False negatives (FN), and True negatives (TN), are presented together in the image as the corresponding confusion matrix. The confusion matrix structure is shown in Fig. 6. The model's performance is better when the positions corresponding to the observations are more in quadrants two and four, and the model's performance is worse when they are more in quadrants one and three.

		Predicted condition	
		Positive(PP)	Negative(PN)
Actual condition	Total Population= P+N		
	Positive(P)	True positive(TP), hit	False negative(FN) type II error,miss, underestimation
	Negative(N)	False positive(FP) type I error,false alarm,overestimation	True negative(TN) Correct rejection

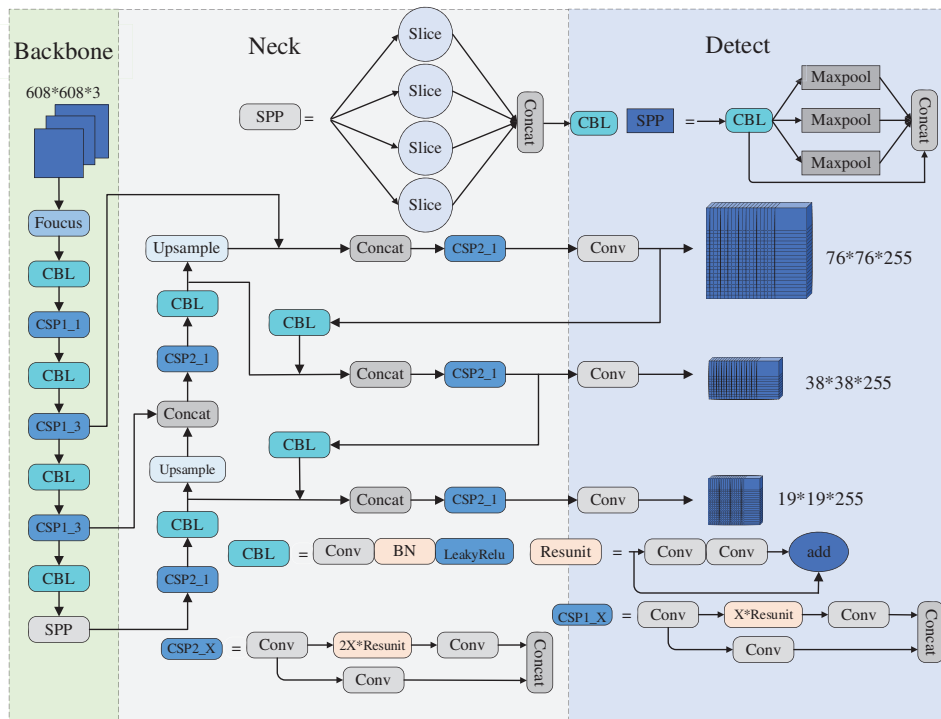
**Figure 6: Confusion matrix**

### 2.1.3 Commonly Used Deep Learning Models

You Only Look Once-V5 (YOLOv5) is the most commonly used deep learning model for orthopedic image recognition. As a real-time detection model, its detection speed and accuracy have been validated on several validation sets with reasonable accuracy. Compared with the previous generation model YOLOv4, the new generation model YOLOv5 has improved in model resource consumption, detection speed and accuracy, and page design. Although YOLOv5 is not the latest achievement of the YOLO series, its balanced recognition speed and accuracy make it widely used. The frame and performance variations of the YOLO series are shown in Table 2. The structure of YOLOv5 is shown in Fig. 7.

**Table 2:** The dataset used for YOLO and YOLOv2 is VOC2007; the rest use COCO2017

Model	Date	Anchor	Backbone	AP
YOLO	2015	No	Darknet24	63.4
YOLOv2	2016	Yes	Darknet24	63.4
YOLOv3	2018	Yes	Darknet53	36.2
YOLOv4	2020	Yes	CSPDarknet53	43.5
YOLOv5	2020	Yes	Modified CSPv7	55.8
PP-YOLO	2020	Yes	ResNet50-vd	45.9
Scaled-YOLOv4	2021	Yes	CSPDarknet	56.0
PP-YOLOv2	2021	Yes	ResNet101-vd	50.3
YOLOR	2021	Yes	CSPDarknet	55.4
YOLOX	2021	No	Modified CSPv5	51.2
PP-YOLOE	2022	No	CSPRepResNet	54.7
YOLOv6	2022	No	EfficientRep	52.5
YOLOv7	2022	No	RepConvN	56.8
DAMO-YOLO	2022	No	MAE-NAS	50.0
YOLOv8	2023	No	YOLOv8	53.9



**Figure 7:** YOLOv5 network architecture

The Focus and Cryptographic Service Provider (CSP) structures proposed by YOLOv5 can improve the receptive field and alleviate problems such as gradient disappearance. However, the model still has some defects, such as image transformation, occlusion, light change, and other indicators that need improvement in complex situations. Because YOLOv5 is a single-stage target detection model, it still faces challenges in the face of orthopedic detection and other small target detection tasks. The current applications of the improved YOLOv5 in medicine are shown in Table 3. At this stage, improvements to YOLOv5 can be made in the following ways. For example, (1) Introduce a multi-task learning mechanism to solve multiple related tasks simultaneously that improves the comprehensive performance of the model. (2) Effectively fuse multi-scale features to improve the detection accuracy of large and small targets. (3) Utilize only weakly supervised signals for detection to reduce the workload of data annotation, thus improving the model's Robustness.

**Table 3:** Current improvements to YOLOv5

Model	Improvements to YOLOv5/Improvement of indicators
YOLOv5-CASP [9]	An improved Convolutional Block Attention Module (CBAM) module was added to the YOLOv5's skeleton and camera, enhancing image detection. It replaced the original Spatial Pyramid Pooling-Fast (SPPF) module with the improved Atrous Spatial Pyramid Pooling (ASPP) module to increase the ability to extract multi-scale contextual information. It replaced the C5 module with the improved Cot3 module to increase the learning ability of self-attention. / MAP increased by 4–5 percent.
YOLOv5-CBD [10]	The redundancy effect on features after fusion is significantly reduced by adding a coordinate attention mechanism to emphasize key features. The feature pyramid structure in feature fusion is replaced with a weighted bidirectional feature pyramid, which achieves funny bidirectional cross-scale connectivity and weighted feature fusion. Finally, a combination of distance intersection and non-extremely significant value suppression is used to solve the problem of the high leakage rate of overlapping objects. / The average accuracy of the model is improved by 4.5% relative to the pre-improvement period.
YARN [11]	The dataset images are first preprocessed for digital enhancement in the training of the dataset by YOLOv5, and finally, the classification of the local images is done using ResNet34. The stochastic gradient descent (SGD) optimizer has been selected for the joint classification training of ResNet34. / An accuracy rate of more than 90 percent for each classification was achieved.
YOLOv5-R [12]	Efficient Channel Attention (ECA) modules in the Ghost module first, reducing redundancy issues. Afterward, dense connections were used to improve the network performance, and the CSPDarknet5 in YOLOv5 was replaced with the F-GED module. Finally, separable convolutional fasts were added to the neck and the head of the model to reduce the computational complexity significantly. / The average accuracy was improved by 3.1%, and the number of floating point operations per second and parameters were reduced by 25% and 47.2%, respectively.

(Continued)



**Table 3 (continued)**

Model	Improvements to YOLOv5/Improvement of indicators
YOLOv5 R6.1 [13]	They replaced the Conv structure in YOLOv5 with an improved Stem structure. The robustness of the model was subsequently enhanced using the on-the-fly erasure data extension technique. After replacing the Spatial Pyramid Pooling (SPP) & CSP structures using SPPF and C3, FPN+PAN32 is finally used for multilevel feature fusion at the neck. / The MAP was improved by 6.5%.
I-YOLOv5 [14]	The Hybrid Grid Search Optimization Algorithm (HGSOA) was combined with Hyperparameter Optimisation (HPO), significantly enhancing the ability to visualize hyperparameter search optimization in deep neural networks. The McCulloch algorithm was also used to localize and segment the images. / The average accuracy reached 91.19%.
YOLOv5-Transformer [15]	Fusing the Transformer with YOLOv5 retains YOLOv5's original ability to extract fine features and improves the ability to extract global feature information. / Accuracy improved by 0.09, recall by 0.01, and F1 score by 0.04.
SW-YOLOv5 [16]	Swin Transformer's sliding window self-attention operation (SW-MS) is employed to enhance the global attention capability of the model, and the image size is linearised to reduce the computational effort. / The MAP value reached 99.0%, an improvement of 8.5%.
KPE-YOLOv5 [17]	The k-means++ technique was used to improve the anchor frames and increase the ability to extract feature information by adding a scSE attention module with a small target detection layer. / The MAP was improved by 5.3%.

UNet was proposed by Olaf Ronneberger et al. in 2015 [18] and is now widely used in medical image segmentation due to its good segmentation accuracy. The network is U-shaped and adopts an entirely symmetric left-right structure. The left side consists of convolutional downsampling and MaxPooling, referred to as the contraction path in the original paper. The right side consists of four blocks, each feature-reduced by upsampling. This approach reduces the feature mapping of the output of the compression path and makes it consistent with the input image, referred to as the extension path in the original paper. The difference between UNet and the traditional segmentation model Fully Convolutional Networks (FCN) for Semantic Segmentation is that the deep and shallow information in FCN is achieved by adding the corresponding pixels. In contrast, UNet is achieved by splicing, which retains more positional information and allows deeper layers to choose freely between shallow UNet, which is more commonly used in the medical image field and requires high semantic segmentation accuracy. The structure of UNet is shown in Fig. 8.

In the deep information, the low-resolution information, after many times of downsampling, can provide the semantic information of the segmentation target in the context of the whole image. In the shallow information, the high-resolution information directly transferred from the encoder to the decoder after the concatenate operation can provide finer features for segmentation. However, because of the compacting path when superimposed on the convolution and pooling operation to gradually reduce the resolution of the feature map, this approach will introduce many parameters, reducing the model's efficiency. Downsampling will continue to lose spatial information, affecting the final segmentation effect, and up-sampling involves spatial information restoration, which is only

possible to achieve by considering the global information. The current stage of the improvement method on UNet is shown in Table 4. The following strategies can be used as future research directions: 1) Construct a global aggregation module to aggregate global information without deepening the structure of the contracting path, which can effectively solve the information loss problem in the up-sampling process. 2) Introducing an attention mechanism or a lightweight network can solve the problem of many UNet parameters and high computation and ensure the model is manageable.

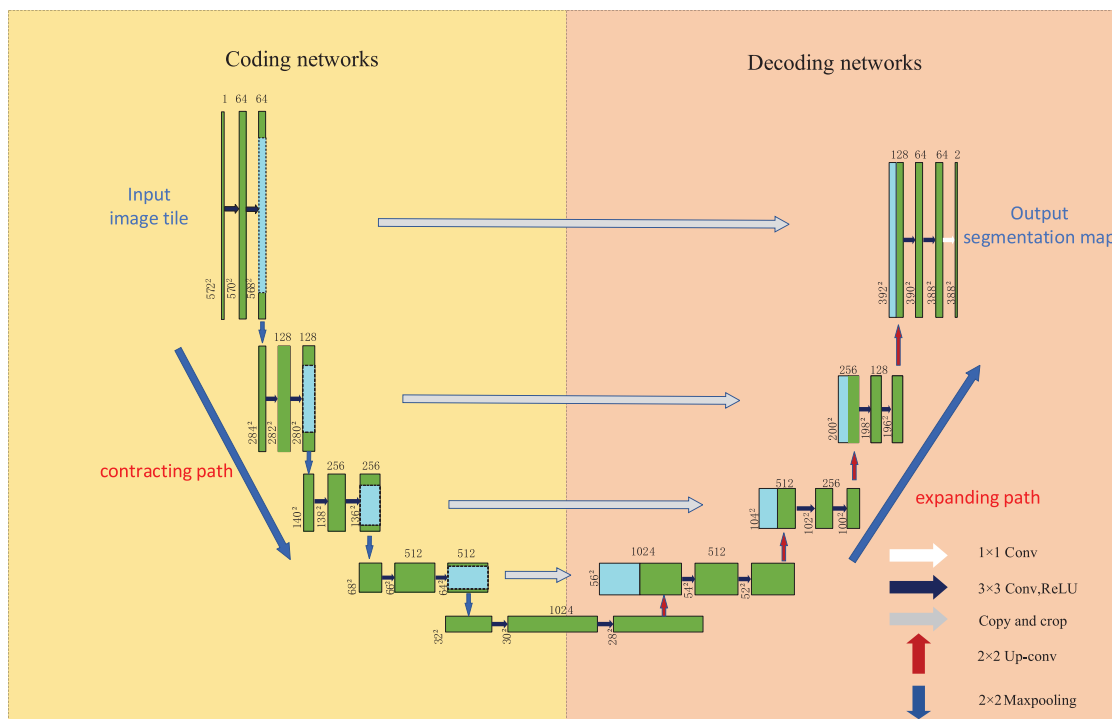


Figure 8: UNet network architecture

Table 4: Current improvements to UNet

Ideological improvements	Model	Date	Dimension	Score
Residual mechanism	V-Net [19]	2016	3D	Avg. Hausdorff Distance score was $5.71 \pm 1.20$ mm
	R2U-Net [20]	2018	2D	The mIOU score is 0.821
	MultiResUNet [21]	2019	2D/3D	5-Fold Cross Validation was $78.1936 \pm 0.7868$
Dense network	FD-UNet [22]	2018	2D	AVERAGE SSIM scores was $0.82 \pm 0.07$
	MDU-Net [23]	2018	2D	Dice score was 0.928
	H-Dense UNet [24]	2018	2D/3D	Dice scores were $0.937 \pm 0.02$

(Continued)

**Table 4 (continued)**

Ideological improvements	Model	Date	Dimension	Score
Feature fusion	CE-Net [25]	2019	2D	IOU scores was 92.63
	MFP-UNet [26]	2019	2D	Dice scores were $0.97 \pm 0.13$
	U-DET [27]	2020	2D	Dice scores was 0.8282
Loss function	BridgedUNet [28]	2018	2D	Dice scores of 89.96
	RAUNet [29]	2019	3D	Miou scores was 0.9562
	AnatomyNet [30]	2019	3D	Avg Dice score was 0.7925
Jump connection	UNet++ [31]	2018	2D	IOU scores was 92.63
	RA-UNet [32]	2019	3D	Dice scores was 0.9771
	ANU-Net [33]	2020	2D	Dice scores were 0.9479–0.9815

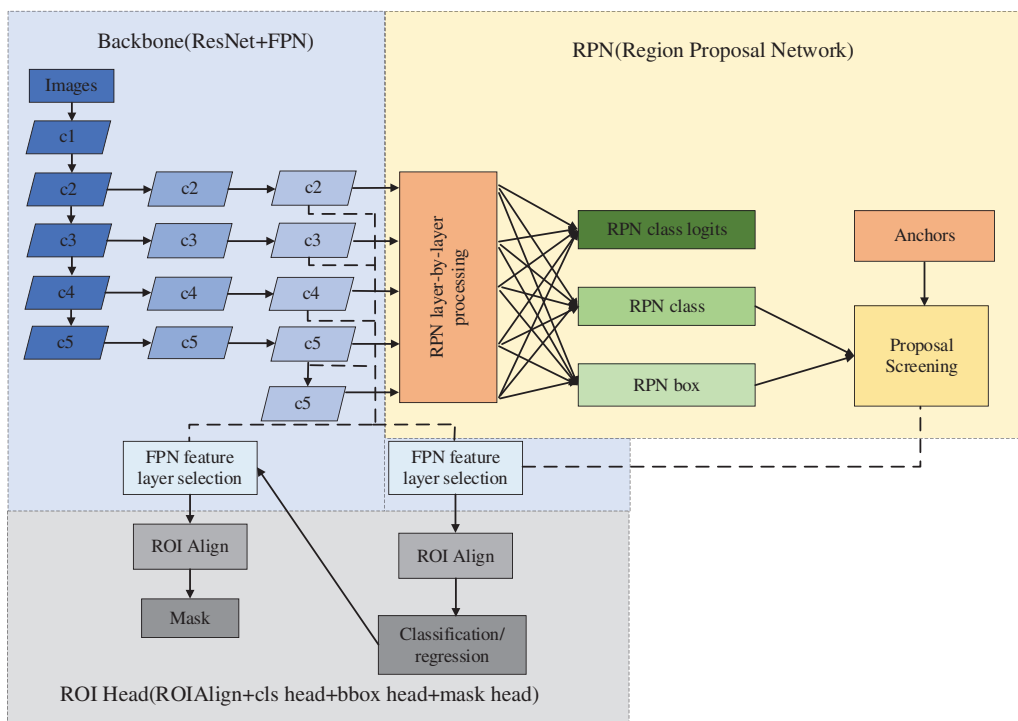
Mask region-based convolutional neural network (R-CNN) was proposed by He et al. [34] in 2017; based on the previous generation of Faster-RCNN, a fully connected segmentation network was added on top of the leading feature network, and the original two tasks (classification regression) was changed to three tasks (classification, regression, and segmentation). Table 5 lists the AP performance of Faster R-CNN and Mask R-CNN with the MS COCO dataset. By comparing the various indexes, it is easy to find that Mask R-CNN is better than Faster R-CNN in all aspects, and the good semantic segmentation and target recognition accuracy of Mask R-CNN makes it favored by medical image researchers. The structure of Mask R-CNN is shown in Fig. 9.

**Table 5:** Comparison of AP performance between faster R-CNN and Mask R-CNN

Model	Backbone	AP <sup>bb</sup>	AP <sub>50</sub> <sup>bb</sup>	AP <sub>75</sub> <sup>bb</sup>	AP <sub>s</sub> <sup>bb</sup>	AP <sub>M</sub> <sup>bb</sup>	AP <sub>L</sub>
Faster R-CNN	ResNet-101-C4	34.9	55.7	37.4	15.6	38.7	50.9
Faster R-CNN	ResNet-50-FPN	37.5	58.7	39.1	21.5	39.7	44.6
Faster R-CNN	ResNet-101-FPN	38.9	60.9	42.3	22.4	42.4	48.3
Faster R-CNN	Inception-ResNet-v2	34.7	55.5	36.7	13.5	38.1	52.0
Mask R-CNN	ResNet-50-FPN	37.5	59.4	40.6	22.1	40.6	46.2
Mask R-CNN	ResNet-101-FPN	39.8	61.6	43.3	22.9	43.2	49.7
Mask R-CNN	ResNetx-101-FPN	39.8	62.3	43.4	22.1	43.2	51.2

The structure of Mask R-CNN is rigorous, in which the Feature Pyramid Network (FPN) network adopts the hopping level connection similar to that in the UNet network, which enhances the ability of multiscale representation and uses the feature pyramid structure to integrate the multiscale information. Then, the high-quality proposal obtained by the prediction of the Region Proposal Network (RPN) network is transmitted to the Region of Interest (ROI) Head structure. Finally, the input feature map is predicted by the FCN layer to get the final mask result. In the year when Mask R-CNN was proposed, it not only won the best paper of ICCV2017 but also achieved better results than the existing model algorithms in the three challenges of the COCO dataset. However, facing orthopedic images, which are mainly segmented by small-sample target instances and lack pixel-level annotation,

the performance index of Mask R-CNN still cannot meet the clinical use requirements. The current stage of the improvement method on Mask R-CNN is shown in Table 6. The following methods could be future improvements: 1) When orthopedic images lack pixel-level labeling, we can consider designing new loss functions or developing active learning methods to reduce the time of manual labeling. 2) When faced with small-sample instance segmentation, we can consider designing new data augmentation methods and introducing migration learning and generative adversarial networks to solve the small-sample segmentation problem.



**Figure 9:** Mask R-CNN network architecture

**Table 6:** Current improvements to mask R-CNN

Model/Date	Improved methodology/Performance improvement
MOM-RCNN [35]/2021	The model adds a migration learning approach to compensate for low data feasibility, improves SGD and Adam optimizers to speed up convergence, and reduces manual pre-processing and post-processing time spent on denoising. / Achieves 92% accuracy and a detection time of just 5 s.
IMaskRCNN [36]/2022	By adding additional ROIAligned modules with the decoder and using jump connections. / The Dice score was improved by an average of 5% compared to the Mask RCNN.

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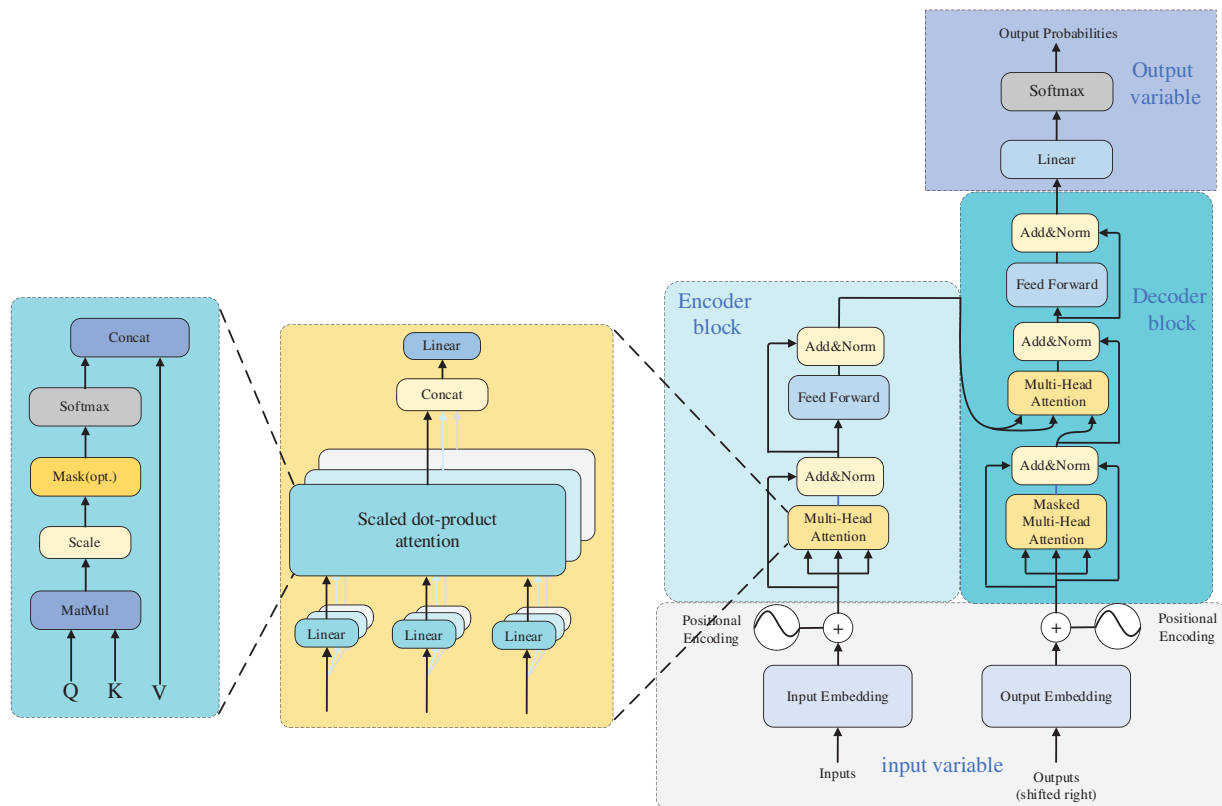
**Table 6 (continued)**

Model/Date	Improved methodology/Performance improvement
P-Mask RCNN [37]/2021	Reduced time and space consumption by removing many invalid anchors, reinforcing feature extraction for small targets, and expanding the anchors in the feature map candidate region. / AP, AP <sub>50</sub> and AP <sub>75</sub> are improved from 37.55%, 77.39% and 33.32% to 41.87%, 81.55% and 41.43%.
Mask-DenseNet+ [38]/2021	The structure of the DenseNet network was adjusted and improved by adding mask processing operations and introducing the idea of integrated learning; the classifier was strengthened by applying random sampling to the data. / The accuracy was improved to 90.61%, the sensitivity to 78.00%, the specificity to 93.43%, and the AUC to 0.9502.
Nuclei R-CNN [39]/2019	Image features are extracted using a deep classification network, and then-candidate regions are predicted using the structure of the FPN network with region proposal class (rp-class) and region proposal bounding box (rp-bbox). Finally, the FCN-like network outputs a binary mask for segmentation. / The results show that the method's accuracy is improved to 90%.
Improved Mask R-CNN [40]/2019	Using Laplace operators to process CT images and ResNet50 and FPN as the backbone of Mask R-CNN, the activation function was replaced with a sigmoid in the RPN layer. / Segmentation accuracy was improved by 7%.
Mask RCNN-FPN [41]/2020	Using ResNet-38 as the backbone structure and aligning RPN to RoI, intersections exceeding the connectivity threshold were computed. / The results show an average accuracy of 0.84 for multiple detection and segmentation and an overall accuracy of 91%.
Mask R-CNN+BiFPN [42]/2022	Changing the FPN to a single-layer BiFPN structure simplifies the bidirectional network by deleting the edges of the original nodes and achieving a higher level of feature fusion. / Sensitivity from 88.2%–91.6% and specificity from 86%–88.7%.
MR R-CNN [43]/2020	Feature fusion is enhanced by constructing a feature pyramid network for feature map transfer summation and replacing the complete convolutional layer with a new semantic segmentation layer. The new semantic segmentation layer enhances the ability to extract global and local information by adding FPN to the mask. / The segmentation accuracy is improved by 2%.
HED-Mask R-CNN [44]/2020	The blurring problem in edge detection is solved by enhancing the underlying prediction using deep supervision in holistically-nested edge detection (HED), thus improving the extraction of image edges. / Dice is 0.94 on CT images and 0.91 on MRI images.

Google proposed a Transformer in 2017 [45]. Transformer has been an emerging structure in recent years; the main difference with traditional Recurrent Neural Network (RNN) and Convolutional Neural Networks (CNN) models is that instead of recursive and convolutional structures, it is entirely based on the attention mechanism and residual connections. The attentional mechanisms contained in the structure have been used with great success in natural language processing (NLP) tasks. OpenAI proposed a series of powerful pre-trained language models, Generative Pre-trained Transformer (GPT), based on Transformer, which achieved excellent metrics in article generation and machine translation NLP tasks. Subsequently, researchers in the field of computer vision ported and applied them to many vision tasks with good results. Its primary applications and time are shown in Table 7. The structure of the Transformer is shown in Fig. 10.

**Table 7:** Important milestones for transformer

Appliance/ Date	Dedicate
GPT-1/ 2018.06	The ability of Transformer to learn word vectors is demonstrated, and the model's performance improves component by component as the number of training sessions increases, and is the beginning of a large-scale language model.
BERT/ 2018.10	The model outperforms humans on both measures in the top-level test of machine reading comprehension and records state of the art (SOTA) performance on 11 different NLP tests. They demonstrated strong capabilities in pre-training and fine-tuning in the NLP domain.
GPT-3/ 2020.05	They launched a large language model with 17.5 billion references and 45 terabytes of training data. It enables it to perform empirically even under challenging tasks, such as writing structured query language (SQL) query statements or JavaScript code.
DETR/ 2020.06	The non-maximum suppression (NMS) post-processing steps and a priori knowledge constraints of the traditional target detection model are reduced, and the target detection task is regarded as a prediction task, which realizes end-to-end target detection, dramatically simplifies the pipeline of target detection and provides a new way of thinking for target detection.
VIT/2020.10	Vision Transformer (VIT) breaks through the limitations of the induction bias that the Transformer lacks to get good migration results in downstream tasks. It opens up the visual Transformer era.
Swin transformer/ 2021.03	A fixed-size block of Vision Transformer samples is divided into different sizes of Windows according to the set parameters. Then, each block is operated independently to improve the computational efficiency significantly. An efficient, flexible, and easily scalable Transformer structure is achieved.
DALL-E-2/ 2022.04	The textual cues are mapped to the representation space by a trained encoder, after which an a priori model generates the image coding, which subsequently captures the semantic information in the text, and the decoder finally generates the image. DALL-E-2 pushes the text-to-image technology to a new level.
ChatGPT/ 2022.11	Using self-attention, it learned to predict probability distributions of human language using large amounts of manually labeled data in a Transformer. It is a cross-genre, large-scale language model that has caused a change in the industry.



**Figure 10:** Transformer network architecture

The structure of the transformer is as follows: firstly, position coding is added to the input variables; the encoder block performs a matrix transformation on the sequence data to obtain  $Q$ ,  $K$ , and  $V$  and then calculates the Attention value; the add module contains the residual block, which serves to prevent degradation in the training of the deep neural network, and the Normalize which serves to speed up the training while improving the stability. The fully connected layer is then a two-layer neural network that first linearly transforms the features, then activates the function by Relu, and finally linearly transforms it so that its dimensionality is unchanged. After repeating the addition and normalization process, the data is fed into the decoder block, which has the same functionality as the encoder block. However, the multi-head attention has an additional masking structure that masks specific values so they do not affect when the parameters are updated. After the data is linearly transformed, Softmax obtains the probability distribution of the output, and finally, the predicted output is obtained.

Transformer has the following advantages over other models: 1. It achieves parallel computation, solves the problem that traditional models can only be computed serially, and realizes parallelization between training samples. 2. It solves the problem of long-term dependence, has a global feeling field, and pays attention to the global information. Self-attention requires only one step of matrix computation to complete the correlation between sequences and does not need to be passed through hidden layers like CNN. 3. It has strong multimodal fusion ability and better robustness. It needs to pass through the hidden layer as CNN does. 4. It has strong multimodal fusion ability and better robustness. It can achieve better results when dealing with images, audio, and this paper, and it also

has specific adaptability in the face of noise or abnormal data. 5. It can deal with complex models and data better. Self-attention can globally model the connection between pixels in different locations, thus capturing the information in the image more effectively. However, Transformer still has the following problems when facing images like orthopedics, which are composed of a small number of datasets and are more concerned with fine-grained features: 1) High computational complexity. Dealing with multi-scale complex images will occupy too many resources, and the number of model parameters is large. 2) Insufficient ability to extract detailed features. As self-attention focuses more on global information, it reduces the ability to extract low-resolution images. 3) Loss of location information. Orthopedic images contain a large amount of spatial information at the pixel level, and the Transformer model cannot take advantage of the order in the sequence, which leads to the loss of positional information, and is not sensitive to fine-grained features, which may lead to weak positioning of the boundary capability.

The current improvements of Transformer in medical applications are shown in [Table 8](#). Future research on Transformer can be carried out in the following areas: 1) Accelerated convergence. Use nested dense hopping connections in the backbone network and incorporate residual networks 2) Reduce the number of parameters to reduce computational complexity. It reduces computation effectively by encoding spatial and channel dimension information with shared weights. Also, consider adding a whole convolutional layer to enhance the linear projection. 3) Improve the extraction of detailed features by adding convolutional blocks to enhance the local spatial information capability.

**Table 8:** Current improvements to transformer

Model/Date	Improved methodology/Limitations/Performance comparison on the synapse dataset
TransUNet [46]/2021	It is the first to apply Transformer to medical image segmentation, and combined with UNet, it retains the high-resolution information and inherits the low-resolution information. Global modeling is achieved. / High computational complexity. / Dice score was 77.48.
UNETR [47]/2022	Global information is effectively captured using the Transformer as an encoder to learn a sequence of input 3D image volumes and is directly connected to CNN's decoder via jump connections. / Insufficient model adaptation capability. / Dice score was 79.04.
TransFuse [48]/2021	Connecting the CNN with the Transformer's encoder in a parallel way captures low spatial detail information in a more shallow way. It fuses the multi-level features of the two branches in the BiFusion module, effectively mitigating the problem of gradient vanishing and decreasing gradient. / Upsampling process loses feature information. / Dice score was 80.31.
MedT [49]/2021	Using gated axial attention and proposing a Local-Global training strategy (LoGo) training strategy, gated axial attention is implemented to control the flow of information, alleviating problems such as Transformer's limitation in the field of small datasets such as medicine. / Lack of multi-scale information representation. / F1 scores improved by 1.32–2.19 percent.

(Continued)



**Table 8 (continued)**

Model/Date	Improved methodology/Limitations/Performance comparison on the synapse dataset
Swin-UNet [50]/2022	A symmetric encoder-decoder system with jump connections is constructed using Swin Transformer as the network backbone, deeper features are generated by fusing multiple Swin Transformer modules and image blocks, and finally, up-sampling is implemented to recover spatial information. / Unable to handle spatial information. / Dice score was 83.48.
DS-TransUNet [51]/2022	An extra encoder is added to Swin-UNet to extract the multi-scale feature representation, and the Transformer Interactive Fusion (TIF) module is proposed to establish the global dependency between different scale features through the self-attention mechanism to achieve the interaction between multi-scale features. / The computational complexity is too high. / The dice's and miou's scores reached 0.868 and 0.806, respectively.

#### 2.1.4 Commonly Used Public Datasets in Orthopedics

Deep learning models usually require large amounts of data to avoid overfitting due to too many parameters. There are not many orthopedic datasets that can be made public due to reasons such as patient privacy and relevant laws. Therefore, in addition to using publicly available datasets to train the model, researchers should also use some internal datasets to test the model to ensure the accuracy of the results. Researchers can also extend the datasets by employing data preprocessing. Commonly used public datasets in orthopedics and their download addresses are shown in Table 9.

**Table 9:** Common public datasets

Source of data sets	Type of data set	Quantities	Download address
NYU langone health	Knee	1500	<a href="https://fastmri.med.nyu.edu/">https://fastmri.med.nyu.edu/</a>
MICCAI 2020RibFrac challenge	Ribs	660	<a href="https://ribfrac.grand-challenge.org/">https://ribfrac.grand-challenge.org/</a>
MRSpineSeg challenge	Spine	192	<a href="https://www.spinesegmentation-challenge.com/">https://www.spinesegmentation-challenge.com/</a>
Verse2020	Spine	30423	<a href="https://verse2020.grand-challenge.org/">https://verse2020.grand-challenge.org/</a>
MURA-1.1	Musculoskeletal	40561	<a href="https://aistudio.baidu.com/datasetdetail/20010">https://aistudio.baidu.com/datasetdetail/20010</a>
RSNA bone Age	Bone age	4360	<a href="https://www.kaggle.com/datasets/kmader/rsna-bone-age">https://www.kaggle.com/datasets/kmader/rsna-bone-age</a>

## 2.2 Artificial Intelligence-Assisted Fracture Detection

Traditional methods of fracture diagnosis include radiographs, computed tomography (CT), and magnetic resonance imaging (MRI). However, it is often difficult for radiologists to quickly and accurately determine the fracture site due to tiny fractures, different irradiation locations, and occult

fractures. Using deep learning for fracture detection can effectively eliminate the interference of human subjective factors and shorten the diagnosis time while improving the accuracy rate [52].

### 2.2.1 Rib Fracture Detection

Traditional rib fracture detection methods use CT images. However, due to the particular anatomical morphology of the rib cage, it takes much time for physicians to recognize traditional CT images. Zhou et al. [53] applied a CNN in rib fracture detection and classification, and the results showed that with the assistance of AI, the physician's accuracy, sensitivity, and diagnosis time were all improved, which demonstrates the feasibility of CNN models for rib fracture diagnosis. However, the model used in this study needed to achieve satisfactory levels of accuracy and recall. Akifumi et al. [54] also developed a computer-aided diagnostic system utilizing deep learning, which was used for rib fracture detection. The model is based on a three-dimensional (3-D) object detection network in a two-stage object detection framework that utilizes 3-D convolution to maximize the extraction of image features. The results show that the algorithm is sensitive enough to quickly detect rib fractures in CT images. Liang et al. [55] developed a deep learning model called FracNet to detect and segment rib fractures using a 900-sheet dataset and showed a sensitivity of 92.9% and a Dice coefficient of 71.5%. The proposed model improves the sensitivity of rib fracture detection and significantly reduces clinical time consumption. However, these studies only realized the dichotomous classification of fracture detection and needed to provide a more detailed classification of the fracture degree, which still has limitations in practical applications. Yang et al. [56] used a convolutional neural network to diagnose rib fractures. They compared the diagnostic efficiency of a deep learning system with that of a radiologist and developed a discriminative model for fractures of different degrees. The system can accurately and quickly diagnose and categorize rib fractures, significantly saving medical resources. The specific indicators of the above study are shown in Table 10.

**Table 10:** Studies related to rib fracture detection

Source /Date	Accuracy/Sensitivity/ Specificity/Diagnostic time	Dedicate	Limitations
[53]/2020	91.1%/86.3%/None/ Reduced by 73.9 seconds	Demonstrating the feasibility of deep learning for rib fracture diagnosis.	Unable to show the anatomical location of rib fracture.
[54]/2022	None/93.5%/None/ None	Developed a computer-aided diagnostic system to reduce pressure on radiologists.	Reduced sensitivity of the computer-aided diagnostic systems.
[55]/2020	None/92.9%/ None/ Reduced by 86.3%	A clinically applicable methodology was established to assist radiologists in their clinical practice.	There may still be false positives or false negatives annotations.
[56]/2022	95.22%/95.01%/ 98.32%/ Reduced by 205 s	The classification models can distinguish between new and old fractures and the presence of malalignment in new fractures.	The system is less specific than radiologists.

### 2.2.2 Spinal Fractures

Traditionally, diagnosing thoracolumbar vertebral fractures (VF) in clinical testing is often applied together with imaging analysis, such as CT or MRI. However, this method is time-consuming and needs to improve detection accuracy. Kazuma et al. [57] applied deep convolutional neural networks (DCNN) to the diagnosis of VF for the first time, using images from 300 different patients to train the DCNN and evaluate the diagnostic accuracy, sensitivity, and specificity of the model at the same time with orthopedic residents, orthopedic surgeons, and spine surgeons. The results showed that DCNN outperformed orthopedic surgeons in all performance metrics. However, DCNN still needs to be improved to increase detection accuracy, and many experienced physicians often infer current symptoms by analyzing the patient's medical history, which is yet to be possible with DCNN. The traditional approach is to train the DCNN directly using 3D images. However, this approach is too complex and computationally expensive and requires a lot of model training. Previously, Lindsey et al. [58] proposed deep-learning methods for fracture class detection on 2D images to address this problem. However, these methods are only based on 2D images and cannot be directly applied to 3D images. There is still room for further improvement in practical application and effectiveness. Kazutoshi et al. [59] proposed multiple 2D real-time detection YOLOv3 methods for pelvic fracture diagnosis. Each 2D-DCNN detects the image in different directions, and for each direction, three 2.5D plate images with different thicknesses are synthesized, and each YOLOv3 model simultaneously detects the fracture candidates in different directions. Finally, 3D crack regions were detected by integrating these crack candidates. The results noted a recall and precision of 0.805 and 0.907, respectively, confirming the feasibility of multiple 2D detection models for fracture diagnosis and significantly reducing the computational cost. However, the study only examined issues such as the presence of fracture without grading the degree of fracture. Li et al. [60] proposed a fracture grade identification method by applying the YOLOv5 network search optimization algorithm for graded diagnosis of osteoporotic vertebral fracture (OVF). By accurately detecting the vertebral position, the system realized the graded fracture diagnosis and achieved an accuracy rate of 96.85%, far more than the 54.11% independently detected by physicians. The specific indicators of the above study are shown in [Table 11](#).

**Table 11:** Studies related to spinal fractures

Source /Date	Type of fracture	Accuracy/Sensitivity/ Specificity/ Diagnostic time	Dedicate	Limitations
[57]/2020	Spinal fractures	86.0%/84.7%/ 87.3%/None	First application of deep convolutional neural networks to cone fractures.	Provides no substantial assistance to physicians in developing medical plans.
[58]/2018	Spinal fractures	95%/91.5%/ 93.9%/None	The model can detect multiple fracture sites.	Model performance is overly dependent on the quality of the dataset.

(Continued)

**Table 11 (continued)**

Source /Date	Type of fracture	Accuracy/Sensitivity/ Specificity/ Diagnostic time	Dedicate	Limitations
[59]/2021	Spinal fractures	90.7%/80.5%/None/ None	Detecting 3D cracked regions by fusing multiple 2D images significantly reduces computational cost.	The degree of fracture is not carefully graded.
[60]/2023	Spinal fractures	96.85%/83.35%/ 94.70%/None	Graded diagnosis of vertebral fractures was made.	No integration with clinical indicators to create a comprehensive intelligent diagnostic model.

### 2.2.3 Intertrochanteric Fractures

Takaaki et al. [61] used an AI-assisted method to diagnose inter-rotor fractures. They used 3346 datasets to train and validate the Visual Geometry Group-16 (VGG\_16) model and showed an accuracy of 95.5%, higher than the 92.2% of orthopedic surgeons. Liu et al. [62] proposed a better Faster-RCNN target detection algorithm for identifying fracture lines in intertrochanteric fractures and compared its performance to the physician level. The study's results showed that the accuracy and specificity of Faster-RCNN were significantly better than previous methods and required only a quarter of the physician's time. However, the study database contained only frontal and lateral hip radiographs and did not apply to diagnosing lateral radiographs, and the results were not validated.

Early detection of incomplete fractures and immediate treatment is one of the critical aspects of medical treatment of atypical femur fractures. However, general practitioners often miss the diagnosis of incomplete fractures. Taekyeong et al. [63] developed an integrated migration learning-based model for detecting and localizing fractures to address this issue. They selected six models (EfficientNet B5, B6, B7, DenseNet 121, MobileNet V1, and V2) for migration learning to avoid the problem of needing more features due to small datasets, which in turn may lead to situations such as overfitting. The study used 1050 datasets (which contained 100 images of incomplete fractures) to train the models, and the three highest accuracy and five highest accuracy models were combined and compared. The results show a high accuracy of 0.998 for the former in recognizing incomplete fracture images, which demonstrates the significant effect of migration learning in classifying and detecting fracture images. However, the inability to evaluate the fracture probability during detection limits its application. The specific indicators of the above study are shown in [Table 12](#).

**Table 12:** Studies related to intertrochanteric fracture

Source/Date	Type of fracture	Accuracy/Sensitivity/ Specificity/Diagnostic time	Dedicate	Limitations
[61]/2019	Intertrochanteric fracture	95.5%/93.9%/97.4%/ None	Demonstrating the potential of deep learning models for recognizing fractures.	It is not possible to determine whether CNN can distinguish fractures by binary classifiers.
[62]/2022	Intertrochanteric fracture	84%–88%/87%–89%/71%–87%/13.20 min shorter than traditional testing	A more advanced Faster-RCNN algorithm outperformed previous studies regarding time and metrics.	Only detects orthopantomograms of the hip joint, not recognizing lateral photographs.
[63]/2023	Atypical femur fracture	98.8%/None/ None/ None	Demonstrates the significant effect of transfer learning in classifying and detecting fracture images.	Inability to assess fracture probability.

#### 2.2.4 Systemic Fractures

Responding to the problem of emergency room medical personnel in recognizing multiple fractures in conventional radiographs that are easily missed and misdiagnosed, Jakub et al. [64] applied deep learning to skeletal radiographs for the first time; they used five publicly available deep learning networks, which they improved, trained on 25,000 wrist, hand, and ankle photographs selected from hospitals to detect fractures, lateral deviations, body parts, and examination views. Comparisons with two senior orthopedic surgeons showed over 90% accuracy in identifying body parts and examination views, 90% accuracy in lateral deviation, and 83% accuracy in fracture detection. Although these metrics are similar to those of physicians, the system error rate increases when dealing with blurred images and a lack of data. Rebecca et al. [65] developed a deep learning system for detecting fractures throughout the musculoskeletal system. The system contained ten convolutional neural networks, each using a tiny variant of the extended residual network architecture<sup>23</sup>. The study used 314,886 datasets, divided into training and validation sets at a ratio of 9:1. Various metrics showed that the system accurately mimicked the expertise of orthopedic surgeons and radiologists in detecting fractures in adult musculoskeletal X-rays, demonstrating better robustness in the face of clinically variant cases and cases considered more challenging by physicians. Takaki et al. [66] applied automated localization and classification of Faster R-CNNs to pelvic, rib, and spinal fractures. It was found that with the help of this model, orthopedic surgeons, especially those with less experience, were significantly more sensitive

to pelvic, rib, and spinal fractures. In addition, the model has good fracture detection sensitivity and accurately detects multiple fractures in humans. However, the study did not cover multiple fractures in the human body and could not fully assist healthcare professionals in detecting fractures throughout the body. The specific metrics of the study are shown in [Table 13](#).

**Table 13:** Studies related to systemic fracture

Source/Date	Type of fracture	Accuracy/Sensitivity/ Specificity/Diagnostic time	Dedicate	Limitations
[64]/2017	Multiple fracture detection	90%/None/None/None	First deep learning application to Skeletal X-Ray Images.	The model recognizes errors when images are blurry and data is lacking.
[65]/2020	Multiple fracture detection	97.4%/95.2%/81.3%/ None	Models are more robust in the face of complex cases.	Excessive collection of unusual regions resulted in a less stable positive prediction rate.
[66]/2022	Multiple fracture detection	64.8%/78.6%/None/ None	They demonstrated better accuracy in detecting pelvic fractures, rib fractures, and spinal fractures.	Unable to detect 3D images.

### 2.2.5 Diagnosis of Subtle Fractures

Liu et al. [67], for the first time, applied AI assistance to X-ray images to aid in the clinical diagnosis of tibial plateau fractures (TPFs). The study found that the AI algorithm recognized TPFs with an accuracy of 0.91, which is close to that of orthopedic surgeons ( $0.92 \pm 0.03$ ), but the recognition speed is 16 times faster than that of physicians. However, the study only focused on fracture line recognition and did not include fracture classification. Seok et al. [68] investigated the ability of deep learning algorithms to detect and classify proximal humerus fractures in anterior shoulder radiographs and compared them with a human group. The results showed that the CNN outperformed general practitioners and orthopedic surgeons, especially when classifying complex fractures, which is the most challenging area for human practitioners to differentiate; the CNN performed better. However, the reliability of the algorithm still needs to be improved. Gan et al. [69] used the Faster R-CNN model to detect distal radius fractures and found that the model had similar diagnostic capabilities to those of orthopedic surgeons. However, due to the small dataset used in the study, the results may not be satisfactory in real-world applications. Choi et al. [70] used a deep learning algorithm with a two-input convolutional neural network in combination with anteroposterior (AP) and lateral X-rays of the elbow to automatically detect pediatric supracondylar humerus fracture and compare it with the

physician's performance. The study results showed lower model specificity and PPV relative to human readers. This series of studies demonstrates the potential of deep learning to diagnose microfracture sites in humans. The specific indicators of the above study are shown in [Table 14](#).

**Table 14:** Studies related to the diagnosis of subtle fractures

Source/Year	Type of fracture	Accuracy/Sensitivity/ Specificity/Diagnostic time	Dedicate	Limitations
[67]/2021	Tibial plateau fracture	91%/90.58%/85%/ 0.56 s	Accurate as a doctor and up to 16 times faster than a doctor.	Failure to categorize the degree of fracture.
[68]/2018	Proximal humerus fracture	65–86%/83%– 88%/94%–97%/None	Indicators are much better than general practitioners when the model classifies complex situations.	Algorithm reliability still needs to be improved.
[69]/2019	Distal radius fracture	90%–96%/ 85%–95%/ 93%–99%/None	Verified that the network still exhibits similar metrics to physicians in limited situations.	The amount of data is too small and the model identification process does not meet clinical realities.
[70]/2020	Supracondylar fracture of the humerus	None/93.9%/ 92.2%/None	Used dual-input convolutional neural and dominated performance against physicians.	The study did not include supracondylar dislocation of the humerus.

The above studies show that deep learning has achieved many advanced results in various types of fracture diagnosis. [Tables 10 to 14](#) summarize the application methods of deep learning in fracture diagnosis in different parts of the human body. Among the various studies mentioned above, the image classification assistance models account for the most significant number, and all of them can automatically classify fractures with high accuracy. However, they are least used in practical clinical applications due to their inability to provide more detailed metric information, such as fracture location and fracture line shape. On the other hand, the research on target detection can obtain both the location and category information of the fracture, which benefits the doctors' diagnosis in the actual clinic. However, it needs to consume more computational resources when dealing with large-scale data, and there is still much room for improvement in speed enhancement. Among the above studies, image segmentation is the least studied. Although image segmentation models can provide more detailed information about fracture contours and anatomical structures, which is more helpful for doctors to determine the scope and severity of fractures in the clinic, it is still challenging to deal with complex scenarios, such as overlap and occlusion between multiple fractures. Therefore, future

research in deep learning applied to fracture diagnosis may focus more on improved aspects of target detection and image segmentation.

### ***2.3 Enhanced Image Features***

Large datasets are often required in AI-assisted fracture diagnostic studies; however, lack of interpretability and imaging ambiguity have been problems faced in past studies. Wu et al. [71], to cope with this problem, proposed the Functional Ambiguity Mitigating Operator (FAMO) model aimed at mitigating the impact of functional ambiguity on fracture detection, which applies to radiographs of a wide range of body parts. This study investigated whether good diagnostic results can be achieved with small datasets. In the study, ResNext 101 + FPN was used as the base network structure, processed with the addition of the FAMO model, and the other group was kept as ResNext 101 + FPN as a control. The study results showed that the FAMO model performed better in sensitivity, specificity, and AUC, with most AUCs exceeding 80% per case in different body parts. The new operator FAMO proposed in the study helps to mitigate feature ambiguity in X-ray fracture detection, thereby improving sensitivity and specificity at the level of per fracture, per image, and per case in all body sites. However, the unbalanced proportion of sites in the dataset and the single data source still need further improvement.

Different forms of fracture cause inaccurate results not characterized by categorization during imaging. To address this problem, Lee et al. [72] introduced radiological reports as additional information in a medical image classification task for the first time. They proposed a neural network with an encoder-decoder structure trained using radiology reports as auxiliary information and applied a meta-learning approach to generate adequate classification features. The network then learned classification representations from X-ray images and radiological reports. The results show a classification accuracy of 86.78% for the training dataset and an F1 score of 0.867 for fracture or standard classification, demonstrating the potential of deep learning to improve performance. However, the dataset's imbalance and the system's generalization ability still need to be improved.

Pawan et al. [73] proposed a data enhancement technique called BoostNet to improve the performance of deep neural networks in a four-step approach: 1. Several deep learning models are compared. Champnet is selected as the base model. 2. Datasets with different resolutions are evaluated to enhance the model performance. 3. The model is combined with image enhancement techniques (constrained self-adaptive histogram equalization, high-frequency filtering, and unsharp masking) to enhance the model performance further. 4. The model performance is verified by luminance order error to validate the BoostNet results. Their classification scheme achieved 95.88%, 94.99%, and 94.18% accuracy in musculoskeletal radiograph bone classification compared to ChampNet + CLAHE, ChampNet + HEF, and ChampNet + UM, respectively. This method demonstrates the feasibility of data enhancement in orthopedic images.

### ***2.4 Assisting in the Diagnosis of Orthopedic Diseases***

Early diagnosis and timely control of diseases are essential for treating patients and saving medical resources. Many diseases are difficult to treat in the later stages and are associated with many sequelae. However, the early diagnosis of many diseases is often complicated, resulting in delayed medical treatment. Applying deep learning in orthopedics frees patients from cumbersome examinations and even realizes remote system consultation for patients while saving medical resources for hospitals, which has significant application value.



### *2.4.1 Scoliosis Detection*

The complex process of traditional scoliosis screening methods, the significant differences in anatomical structures of patients of different ages, and the low tissue contrast of X-ray spine images lead to inaccurate manual observation of the spinal curvature. At the same time, the patients are also at risk of radiation exposure. To address this problem, Yang et al. [74] developed a deep learning algorithm, a model that automatically screens for scoliosis on images of a patient's back after removing clothing. The results show that the algorithm outperforms professional physicians in detecting scoliosis and grading severity. Patients can be screened remotely without being exposed to radiation risks. The study also showed promising results in initial diagnosis and prevention. However, the dataset used in the study needs to be more homogenous, containing only confirmed cases. In addition, the images used in the study were two-dimensional, and the image dimensionality enhanced to improve the model's accuracy is an area that could be improved in the future. Ananthakrishna et al. [75] proposed an accurate computer-based automated measurement method that estimates spinal curvature based on identified anatomical landmarks and categorizes the scoliosis into four grades, which helps to minimize subjective errors and shows good accuracy during testing.

### *2.4.2 Detection of Lumbar Disc Degeneration*

Traditional lumbar disc detection is too complicated and lacks quantitative standards. Zheng et al. [76] proposed a T2MRI-based lumbar disc degeneration (IVDD) segmentation network and quantification method, which consists of three modules and can realize high-precision segmentation of the IVDD region. The study demonstrated the relationship between lumbar disc degeneration and patient information that developed quantitative criteria for IVDD. This quantitative standard supports clinical trials and scientific research while also improving the efficiency of patient care. However, the study was limited to a trial in China, so the results may not be applicable globally.

### *2.4.3 Osteoporosis Detection*

In response to the high price of dual-energy X-ray bone densitometry for osteoporosis diagnosis and its limited availability in developing countries, Ryoungwoo et al. [77] applied deep learning model for the first time to the study of the acceptable diagnostic outcome of osteoporosis. They used a deep learning algorithm to predict osteoporosis by using simple hip radiography and built a deep neural network model. They randomly selected 1001 images and divided them into a training, validation, and test set. Modules such as external validation and attention mechanisms were also introduced. The study showed that the model achieved satisfactory results in all indicators and external validation, proving that the deep learning network model has potential value as a screening tool in osteoporosis diagnosis. However, due to the small dataset, it was impossible to classify the images into three categories (normal-osteopenia-osteoporosis). It only dichotomized the images, a significant limitation in practical applications. In addition, the subjects in the dataset were limited to postmenopausal middle-aged women, which is not generalizable in the scope of the group targeted.

### *2.4.4 Hip Detection*

Traditional methods for detecting developmental dysplasia of the hip (DDH) tend to have low accuracy when targeting children's pelvic anatomy. Zhang et al. [78] applied deep learning to anterior pelvic radiographs to diagnose DDH in children. Compared with clinician-led diagnosis, the deep learning system was highly consistent, more convenient, and effective in DDH diagnosis. On top of that, Hiroki et al. [79] further improved the model by using YOLOv5 for DDH detection for the

first time, developing a deep learning model in combination with a single-shot multi-box detector (SSD), and introducing migration learning. The dataset contains 205 standard images and 100 DDH images. The experimental results show that the sensitivity and specificity of the model are 94% and 96%, respectively, and the model also outperforms the standalone SSD model. However, there is still room for improvement with the limited number of datasets and the level of object detectors.

#### 2.4.5 Cervical Spinal Cord Detection

Merali et al. [80] used a deep learning approach for the first time to detect degenerative cervical myelopathy (DCM) [81]. The model used a ResNet-50 neural network with class activation maps and used 6588 images to construct the dataset. It was found that the model performed well in detecting spinal cord compression in cervical MRI scans. Furthermore, in clinical trials, the model could automatically encode MRI scans for automatic feature extraction and generate data for secondary analysis, demonstrating the feasibility of training existing CNNs in new medical imaging classification tasks. However, the dataset contains only confirmed cases and lacks images of normal and mild patients. In addition, peripheral spinal cord compression was not differentiated during dataset labeling, which may trigger clinical symptoms in practical use. Therefore, improvement and categorization of the dataset are the following steps to be considered in this study.

Patients with spinal cervical myelopathy (CM) are often delayed in optimal treatment due to the lack of early symptoms. Eriku et al. [82] developed a machine-learning-based case screening method to address such problems. They proposed a technique for early detection of CM that encourages patients to consult a spine specialist to confirm the diagnosis and receive early treatment. The data was analyzed to screen out patients with CM by recording the differences in drawing time and drawing pressure between patients with CM and normal subjects when depicting spiral, square, and triangular waves on a tablet computer. The results showed that the model had a sensitivity and specificity of 76% in identifying whether a patient had CM, with an AUC of 0.80. However, other writing-motor disorders that could affect the results were not analyzed, and the method lacked sufficient sensitivity for further research to improve it for clinical use. A detailed description of the above essential studies is shown in [Table 15](#).

**Table 15:** Relevant studies and their indicators

Source/Date	Type of disease	Accuracy/Sensitivity/ Specificity/PPV/NPV	Dedicate	Limitations
[74]/2019	Scoliosis	77.8%– 82.1%/85.7%/89.6%/ 85.2%/None	Patients avoid the risk of radiation exposure and outperform medical professionals.	The 2D images used resulted in poor accuracy.
[76]/2022	Degeneration of the lumbar disk	88.89%–90.27%/ 90.99%–95.40%/ None/None/None	Development of quantitative standards for IVDD and high-precision segmentation of the region.	Results in too small a group of applicants.

(Continued)

**Table 15 (continued)**

Source/Date	Type of disease	Accuracy/Sensitivity/ Specificity/PPV/NPV	Dedicate	Limitations
[77]/2021	Osteoporosis	81.2%/91.1%/68.9%/78.5%/86.1%	Reduced costs of osteoporosis diagnosis and good results on indicators.	There is no careful delineation of the classification of osteoporosis and to whom it applies.
[79]/2023	Hip joint	None/94%/96%/None/None	YOLOv5 was introduced for detection migration learning, and the model showed promising results.	The dataset is too homogenous, and the detector level could be improved.
[80]/2021	Cervical degenerative myelopathy	94%/88%/89%/None/None	The model can automatically encode MRIs, significantly reducing the physician's workload.	Failure to delineate cases in detail.
[82]/2023	Spinal Cervical Spondylosis	80%/76%/76%/None/None	Proposed technology for early detection of CM, saving medical resources.	Lack of sensitivity and failure to analyze the effect of other diseases on the results.

#### 2.4.6 Knee Joint Testing

Knee osteoarthritis (KOA), a common musculoskeletal disorder, is currently limited to medical treatment for symptomatic relief and total joint replacement surgery. Therefore, successful prediction of KOV progression would save millions of patients from surgery. However, conventional methods are usually subjective in their estimation of symptoms and radiographs, and therefore, an objective adjunct system is needed to help physicians make the diagnosis.

Aleksei et al. [83] proposed a multimodal machine learning-based KOA progression prediction model, which directly utilizes raw radiological data, physical examination information, patient history, anthropometric data, and optional radiologist statements (KL level) to predict the progression of structural KOA. By using 3,918 images for the test evaluation, they obtained an area under the ROC curve of 0.79 and an average accuracy of 68%, which gives the model a clear advantage in all metrics compared to reference methods such as logistic regression. However, the method is too dependent on the KL classification system and a single dataset, which needs improvement. Subsequently, Bany Mohammed et al. [84] proposed a CNN model and interpretable ensemble consisting of three modules.

The ensemble included a scale-invariant and aspect-ratio-preserving model for localizing the knee joint and created multiple instances of a “hyperparameter-optimized” CNN model. In addition, they created an integrated scoring system based on the Kellgren-Lawrence grading (KL) scale to assess the severity of KOA and provide visual interpretation to predict disease progression. They tested the model using 37,996 datasets, and metrics showed that the method performs best in current KOV testing. However, the method has some limitations, such as low performance in classifying  $KL = 1$ , duplicate data in the dataset, and over-reliance on X-rays. Hegadi et al. [85] used ANN to differentiate between X-ray images of healthy and diseased knees, extracted the synovial cavity region from the images, and calculated the curvature values using noise cancellation and image enhancement techniques, which were shown to be 100% accurate. However, the experiment used only 42 datasets, making it possible for the results to be highly biased.

Knee joint effusion is a common trigger for knee osteoarthritis; however, traditional methods for effusion detection are costly. Sandhya et al. [86] developed a high-density neural network model. They trained and evaluated the network’s performance using low-resolution images to investigate the model’s applicability in low-cost MRIs. They validated the model with 163 validation sets and checked the stability of the model by adding zero-mean Gaussian noise to the test images. The results showed that the model’s accuracy only decreased by 1% in the presence of interference. Compared to the VGG16 network, the model demonstrated a significant advantage in distinguishing between normal and high fluid levels, and its overall performance outperformed that of radiologists. The feasibility of using neural network models for detection at low-resolution images was confirmed. However, the dataset used in this experiment is relatively tiny. Further model training and parameter optimization will be valuable directions for future work.

#### 2.4.7 Bone Tumor Detection

Bone tumors are classified as benign and malignant, and the treatments differ. Benign tumors can be cured entirely by small resection of the tumor and have a better prognosis. Malignant tumors, on the other hand, require extensive surgery with chemotherapy and other methods and have a poorer prognosis [87]. Therefore, it is crucial to accurately determine the degree of malignancy of the tumor at the initial stage of treating the patient. Nonetheless, traditional bone tumor diagnostic methods such as CT, X-rays, and MRI cannot identify complex and subtle bone tumors well. The application of AI in bone tumor detection and diagnosis has the advantages of fast speed, high accuracy, and identification of complex tumors. It has gradually begun to be applied in the clinic.

Kaito et al. [88] proposed a method to automatically assess bone tumors’ benign or malignant nature using deep learning and compared two networks, VGG 16 and ResNet 152. The experimental results showed that VGG 16 had better results in terms of recall and accuracy. In diagnosing six benign and four malignant patients, the model successfully classified them correctly. However, it requires physicians to manually segment the images, limiting its application in the clinic. Vlad et al. [89] used two pre-trained residual convolutional neural networks to classify images extracted from an MRI dataset for two classifiers, T1 and T2. It is worth noting that the amount of data used for the T1 classifier is twice that of the T2 classifier. Clinical trials have confirmed that the T1 classifier outperforms the T2 classifier, and both classifiers enable automatic segmentation of MRI images, thus significantly reducing the workload of physicians. However, these studies were limited to classifying bone tumors into benign and malignant categories, which could not solve practical clinical problems. Li et al. [90] developed a deep learning model called YOLO, which can detect and classify bone lesions on full-field radiographs with limited manual intervention. They trained the model using 1085 bone tumor radiographs and 345 normal bone radiographs. In the detection task, the model’s accuracy on the

internal and external validation sets was 86.36% and 85.37%, higher than the two radiologists' 81.87% and 79.27%, respectively. In addition, physicians in clinical practice favor the model's ability to detect typical, benign, neutral, and malignant tumor types.

Biopsy necrosis rate is the traditional method of measuring bone tumor sensitivity and guiding postoperative chemotherapy. However, studies have shown that this invasive procedure carries risks for patients [91]. For this reason, Xu et al. [92] proposed a new method for detecting necrosis rates using time-series X-ray images. This method utilizes a generative adversarial network with long and short-term memory to generate time-series X-ray images, and an image-to-image transformation network produces an initial image. This method enlarges rare bone tumor X-ray images by a factor of 10, resulting in necrosis rate grading results similar to biopsy. It is the latest technique for detecting rare bone tumors' necrosis rate, overcoming conventional methods' time-consuming and invasive problems.

#### 2.4.8 Orthopedic Rare Class Disease Detection

Zafer et al. [93] proposed a new method for training deep neural networks with limited data to address the problem of a limited number of rare disease datasets. They trained CNN models by modifying data created from normal hip radiographs. Patient images were not used in the training phase, and Legg-Calve-Perthes disease (LCPD) images were tested in the testing phase. The results showed the method was more accurate than the experimental specialized physicians. However, due to the scarcity of datasets, test and training data were mixed in the experiment. In addition, the accuracy of the model results was somewhat affected because only the height of the femoral head was changed, especially the lateral column. Nonetheless, this experiment provides valuable lessons for researching rare diseases in orthopedics.

A detailed description of the above important studies is shown in [Table 16](#).

**Table 16:** Relevant studies and their indicators

Source/Date	Type of disease	Accuracy/Sensitivity/ Specificity/PPV/NPV	Dedicate	Limitations
[83]/2019	Osteoarthritis of the knee	68%/None/None/ None/None	The proposed method predicts knee osteoarthritis progression, thus helping to implement personalized medicine.	Models over-rely on the KL grading system and ignore symptoms of osteoarthritis progression.
[84]/2021	Osteoarthritis of the knee	82%–97%/94%/ None/None/None	A scoring system was developed, and the severity of osteoarthritis of the knee was carefully categorized.	Poor performance in categorization with classification system KL = 1.

(Continued)

**Table 16 (continued)**

Source/Date	Type of disease	Accuracy/Sensitivity/ Specificity/PPV/NPV	Dedicate	Limitations
[86]/2022	Knee joint effusion	61%/None/None/ None/None	Improved model immunity and better overall performance than radiologists.	Does not work well with highly blurred images.
[89]/2022	Bone tumor	80.56%/95.52%/None/ None/None	Comparing two classifiers and achieving automatic segmentation of MRI images.	No careful classification of bone tumors.
[90]/2023	Bone tumor	85.37%/87.10%/None/ None/None	Classifies lesions in detail and outperforms radiologists.	Inadequate consideration of influencing factors and high hardware requirements.
[92]/2022	Bone tumor sensitivity	90%/86.8%/None/ None/None	Overcomes the time-consuming and invasive nature of traditional methods.	The model's true positive indicators still need to be high.

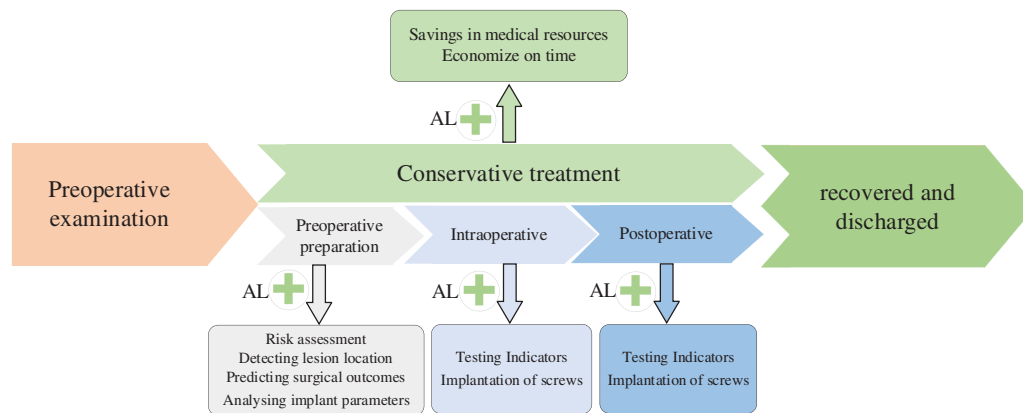
The above studies show that machine and deep learning have achieved good results in diagnosing orthopedic diseases. Tables 15 and 16 summarize the methods and metrics for applying deep learning to diagnose diseases. The 2D images in the above studies are the most extensive and perform well in accuracy. However, 2D images cannot provide more detailed information about the lesions of the disease in practical applications and, therefore, perform poorly in actual clinical results. More importantly, most of the above studies have generally low-quality datasets and severely limited study subjects, which still have significant limitations in clinical applications. Therefore, future studies applying deep learning and machine learning to diagnose orthopedic diseases may focus more on image upgrading and dataset quality improvement.

### 3 Progress in the Application of Artificial Intelligence in Orthopedic Surgery

In recent years, with the development of orthopedic surgery concepts toward refinement, minimal invasiveness, and low risk, the application of AI to orthopedic surgery has become an area of great interest. Applying deep learning, machine learning, and robotics to surgery improves surgical safety and reduces radiation exposure to doctors and patients, which plays a crucial role in the rapid recovery of patients after surgery and reduces surgical stress for doctors.

### 3.1 Deep Learning to Reduce Orthopedic Surgery Risks

In orthopedic surgery, preoperative prediction of surgical risk, clarification of lesion location, analysis of implant parameters, and constant monitoring of intraoperative patient physiology and postoperative recovery are all critical steps. The general flow of spinal surgery is shown in Fig. 11. However, the preoperative, intraoperative, and postoperative stages of traditional orthopedic surgery are the sole responsibility of the physician, which may lead to miscalculations when the physician is inexperienced or overburdened with work. Once the link error occurs, it will seriously affect the patient's surgical outcome. Applying deep learning to orthopedic surgery can alleviate the above problems and reduce medical errors.



**Figure 11:** Flow chart of spine surgery

#### 3.1.1 Preoperative Prediction of Risk

Preoperative prediction of surgical outcomes and risk assessment are integral to the surgery. Incorrect risk assessment can result in additional care or readmission of patients after surgery, which imposes a significant economic burden on the healthcare system [94]. PremN and other researchers [95] developed machine learning algorithms based on preoperative big data for predicting hospitalization time and cost of postoperative patients and proposed a model that takes into account the patient's risk of comorbidities, who trained their model using data from 122,334 postoperative patients, and found that the machine learning algorithm demonstrated excellent validity, reliability, and responsiveness concerning age, race, gender, and comorbidity scores ("risk of disease" and "risk of morbidity"). These tools are expected to support physicians as they develop surgical plans for their patients, helping to identify potential risks, avoid them, and predict possible complications.

#### 3.1.2 Intraoperative Assisted Surgery

Spinal deformities are usually accompanied by various problems such as scoliosis, kyphosis, vertebral rotation, and wedge degeneration, which will make the corrective plan for the patient exceptionally difficult if the location of the lesion cannot be accurately known before the operation. Still, it is often difficult to comprehensively observe the specific information about the location of the lesion by traditional detection methods [96]. Chen et al. [97] proposed a vertebral body that can automatically locate and identify the vertebral body in the three-dimensional CT volume of the Joint CNN learning model (J-CNN), which is based on an initial set of vertebral centroids generated by a random forest classifier. J-CNN can identify vertebral body types and exclude false detections effectively. It was also validated on the MICCAI 2014 Vertebral Bone Localization and Recognition

Computational Challenge dataset, which showed an improvement in recognition rate of 10.12% compared to the state-of-the-art method at that time. This method helps physicians to locate vertebral positions quickly and accurately in the clinic.

With the wide variety of joint replacement prostheses available, traditional methods could be slow to match the patient's prosthesis and have a large margin of error, making it challenging to achieve optimal results with joint surgery. Myriam et al. [98] analyzed the geometric parameters of the implants and the stress shielding effect by combining machine learning with parametric finite element analysis to achieve the optimal performance of the short-shanked prostheses. The study's results showed that the total length of the implant shank is not the only parameter that affects stress shielding; the radius and width of the implant stem also influence the results. This method is faster and more accurate than conventional techniques and contributes to the implant's long-term efficacy.

### *3.1.3 Postoperative Testing Indicators*

Inaccurate placement or inadequate fixation of the implant may lead to dislodgement of the prosthesis and infection of the surrounding tissue. Therefore, imaging analysis of postoperative implants is critical. Traditional methods require X-rays to diagnose postoperative mechanical loosening, but recognizing X-rays may be difficult for inexperienced physicians [99]. Borjali et al. [100] developed an automated tool to detect postoperative mechanical loosening by training deep convolutional neural networks using X-rays. They elaborated on the CNNs learning process that explains how the system works. This research has increased the confidence of healthcare professionals in applying AI in clinical practice.

Álvaro et al. [101] first proposed a multivariate algorithm called AI-HPRO, which combines Natural Language Processing (NLP) and Extreme Gradient Boosting. They applied it to the detection of surgical site infections in patients undergoing hip replacement surgery to solve the problem of time-consuming and resource-consuming detection of traditional surgical site infections (SSIs). The method screens for SSIs in hip replacement surgery patients by combining NLP and extreme gradient boosting. The results of the study show that the clinical indicators are even better than manual testing, where the monitoring time is reduced from 975/h to 63.5/h, and the total number of clinical records manually reviewed is reduced by 88.95%, which is a significant saving of healthcare resources. The study demonstrated that an algorithm combining NLP and extreme gradient boosting techniques can achieve accurate real-time monitoring of orthopedic SSIs.

The above studies show that machine learning and deep learning have achieved satisfactory results in assisting orthopedic surgery. However, despite the excellent performance of the above models in terms of metrics, only a few studies have been carried out in clinical applications. Most studies still suffer from the black box problem, where doctors are not aware of the model and may be reluctant to follow the recommendations of the AI model because the model does not have a human-computer interface, resulting in unintuitive results and the inability to ask questions. Moreover, the EU addressed the liability issue by including a provision in the General Data Protection Regulation that AI algorithmic decisions about humans must be interpretable [102]. Therefore, future research on machine learning and deep learning in assisting orthopedic surgery should focus on the interpretability of the model and develop an assisted diagnostic system; the development of an assisted diagnostic system can help doctors understand the principles of the model more intuitively and the inclusion of an interpretable module in the model can solve the corresponding legal issues.



### 3.2 Robotics in Orthopedic Surgery

Most orthopedic surgeries require the implantation of prostheses due to the complex structure of the human skeleton and its proximity to vital blood vessels. However, inaccurate implant placement due to instrument tremors is inevitable when surgeons are exhausted [103], thus increasing the difficulty of surgery. Therefore, AI-assisted analysis and pathologic judgment are critical to assist surgeons in determining the optimal surgical path and reducing surgical errors [104]. In addition, the rigidity of the human skeleton allows the robot to fixate implants quickly, and the robot's navigation system enables it to handle implants more accurately than the surgeon. Moreover, the camera-manipulated robot provides a stabilized image of the surgical area, which can improve the stability and accuracy of the surgeon during surgical manipulation, thus improving the safety and reliability of the surgery, surgical success, and prognostic outcomes. Considering the general exposure risk to the surgeon in modern surgical procedures, using robots in the necessary part of the surgery can reduce the risk to the healthcare provider. The metrics that should be considered for orthopedic surgery are shown in Table 17; the higher the total score, the better the surgical outcome. As early as 1985, Kwoh et al. [105] began using robots in surgery; however, surgical robots were not introduced into orthopedics until 1992, which stemmed from a collaboration with the U.S. Food and Drug Administration. In recent years, the results achieved by robots in orthopedic surgery have been quite remarkable. Table 18 lists the companies represented by today's orthopedic surgical robots and their products. Pictures of the da Vinci V and Tiangui II Orthopedic surgical robots are shown in Figs. 12 and 13.

**Table 17:** Surgical indicators

Indicator	Interpretations
Performance of implants	Indicators include implant accuracy, stability of fixation, etc.
Post-operative recovery time	Somewhat representative of the outcome of the surgery and also reflects the cost of the patient's post-operative care
Mayo	A composite score of four items: pain, functional status, mobility, and grip strength
VAS	Rating of pain level, with lower scores indicating less pain
Surgical time	Reflects the efficiency of orthopedic surgery
Intraoperative bleeding	Intraoperative bleeding directly affects the probability of infection of the surgical incision
Number of inspections	Reflects to some extent the radiation exposure dose to patients and healthcare workers

#### 3.2.1 Robot-Assisted Navicular Fracture

Fractures of the navicular bone of the hand can affect the movement and stability of the wrist joint of the organism. If the patient does not use the correct treatment in time, it can lead to osteonecrosis, chronic pain, traumatic arthritis, and other serious consequences. Traditional medical methods can lead to sequelae such as postoperative dysfunction [106]. To address these issues, Wang et al. [107] designed an automated multi-degree-of-freedom (DOF) surgical robot with a computer-assisted navigation system for verifying the accuracy of percutaneous navicular bone guides and performed experimental studies on cadavers. The results showed that the method achieved the expected results. Xiao et al. [108] compared the effectiveness of unarmed vs. robotic assistance in the

medical treatment of navicular fractures by recording metrics from different procedures and showed that the robotic-assisted group had significantly better accuracy, shorter time, and less radiation exposure. Wang et al. [109] investigated whether robot-assisted percutaneous screw internal fixation could be used to treat navicular fractures. Patients undergoing robotic-assisted surgery were compared to those undergoing conventional incisional reduction and internal fixation (ORIF) of the navicular fracture. At subsequent postoperative follow-ups, implant accuracy VAS scores were superior to those of the conventional procedure in both the robotic-assisted group.

**Table 18:** Orthopedic robot representative companies and their products

Company identification	Country	Representative product
Intuitive Surgical	American	Da Vinci V
TINAVI	China	Tiangui II Orthopedic Surgery Robot
Stryker	American	RIO Joint Replacement Robot
Yuanhua Intelligent Technology (Shenzhen) Co.	China	Rotary Full Orthopedic Surgical Robot
Zimmer Biomet Holdings	American	ROSA Knee
Microport	China	Honghu Orthopedic Surgical Robot
Medtronic	American	MAZOR X



**Figure 12:** Da Vinci V



**Figure 13:** Tiangui II orthopedic surgical robot

### 3.2.2 Assisting Femoral Surgery

Surgery has been a challenge for physicians in patients with intertrochanteric fractures who often suffer from post-traumatic stress and various underlying conditions caused by surgical intolerance [110]. Reducing operative time, bleeding, and implant accuracy has been the research direction in this procedure. Maeda et al. [111] developed a femoral fracture reduction robotic system called “FRAC-Robo” to assist in dissection and maintenance of reduction during orthopedic surgery. Clinical trials have shown that the robot can generate sufficient force and torque to reduce intertrochanteric fractures, thus confirming the device’s effectiveness in reducing intertrochanteric fractures. Ye et al. [112] proposed a system for robot-assisted femoral fracture repositioning, designing actuators whose trajectories are all linear and whose low-speed and smooth characteristics make them preferable for femoral fracture-type surgeries. A robot-assisted surgery group and a freehand control group were also set up. The study results showed that the number of fluoroscopies, operation time, intraoperative bleeding, and postoperative recovery were better in the robotic group than in the freehand group. A detailed description of the above essential studies is shown in Table 19.

**Table 19:** Relevant studies and their indicators

Source/Date	Type of assisted surgery	Surgical indicators	Dedicate	Limitations
[107]/2023	Navicular fracture	The operation time was 29.1 min, the positioning error was 2.0 mm, and the angular deviation was 3.6°.	Percutaneous navicular bone guide insertion by an automated surgical robot is feasible.	None.

(Continued)

**Table 19 (continued)**

Source/Date	Type of assisted surgery	Surgical indicators	Dedicate	Limitations
[108]/2023	Navicular fracture	Radiation time was reduced by 14 min, operative time was reduced by 16 min, Mayo scores improved by 2%, and postoperative recovery time was reduced by one week.	Feasibility of robotic assistance in navicular fracture surgery demonstrated by comparative experiments.	Small samples and short follow-up periods.
[109]/2023	Navicular fracture	The American Orthopedic Foot and Ankle Society (AOFAS) hindfoot score and VAS score were $(92.25 \pm 2.22)$ and $(0.75 \pm 0.25)$ , respectively.	Robotic assistance is effective in reducing complications and patients recover faster after surgery.	Surgery for robot-assisted repositioning of simple fractures only.
[111]/2008	Femoral surgery	The traction force applied to the lower extremity was 215.9 N, and the internal and external hip rotation torque was 6.7 Nm vs. 6.30 Nm.	Development of a robotic system for assisted femoral fracture surgery and demonstration of its clinical effectiveness.	None.

### 3.2.3 Assisted Total Knee Arthroplasty

In 1972, Insall [113] proposed total knee arthroplasty to reconstruct the patient's joint, correcting the problem of joint deformity and enhancing knee mobility. However, conventional joint replacement surgery is associated with a high risk of postoperative pain, limited postoperative mobility, and poor postoperative rehabilitation. Therefore, the current technology's problem is how to minimize the incision and enhance surgical precision [114]. Robot-assisted total knee replacement, on the other hand, breaks through the limitations of traditional surgery and outperforms it in terms of precision and incision.

Matjaz et al. [115] investigated a robotic system for total knee replacement (TKR) surgery. Preoperative planning software based on computed tomography enabled accurate surgical procedure planning. During the procedure, the surgeon guides a small specialized robot called Acrobot. The robot limits the motion to a predefined area by active constraint control, which allows the surgeon to guide the robot to make ankle cuts for high-precision TKR installation. The system has been successfully applied in seven clinical trials with satisfactory results.

Werner et al. [116] introduced the robot into total knee arthroplasty, and their study found that the mean difference between preoperatively planned and performed postoperative tibio-femoral alignment in the robot group was 0.88, which was significantly lower than that in the conventional control group, which was 2.68. This result suggests that the robot has a promising future for use in

total knee arthroplasty. However, the problems of long operation times and excessive costs still need to be solved.

Cobb et al. [117] compared the results of the Acrobot system with conventional surgery in unicompartmental knee replacement. Their study found that in all patients in the Acrobot group, the tibia and femur were aligned within 2° of the planned position in the coronal plane. In contrast, only 40% of the patients in the conventional group achieved this accuracy. Although the scoring system was subject to a large margin of error and did not allow for extended observation of the patient's postoperative recovery, it still demonstrated that the procedure was less risky and invasive with robotic assistance.

#### 3.2.4 Assisted Spinal Surgery

The complex anatomy of the spine, surrounded by the immediate vicinity of vital blood vessels and nerves, makes spinal surgery difficult. Pedicle screw instrumentation has been the gold standard technique for spinal screw fixation since its introduction by Roy Camille in 1970 [118]. Although pedicle screw instrumentation has been clinically effective, misplaced screws continue to cause severe neurovascular injury. In conventional clinical spine surgery, screw misplacement rates are as high as 15.7% [119]. In recent years, with the development of spinal surgical techniques and concepts, spinal surgery has made significant progress in precision, minimally invasiveness, and postoperative recovery. However, current techniques still need help with radiation exposure and nail placement accuracy.

Ponnusamy et al. [120] introduced the da Vinci robot into posterior spine surgery for the first time and tested it on a porcine model. The study results show that the robot can perform major non-instrumented maneuvers in the posterior part of the spine, enhancing the procedure's safety while reducing the surgeon's stress during the operation.

Addressing the relatively low accuracy of pedicle screws and the need to improve surgical safety, Onen et al. [121] studied the clinical and imaging outcomes of spine surgery in 27 patients by using Spine-Assist and setting up experimental and control groups. The results of the study showed that robotic spine surgery provided high accuracy in pedicle screw placement and significantly reduced radiation exposure. However, robotic-assisted surgery is expensive and may still need help in practical rollout. Lin et al. [122] addressed the problem of the high cost of surgery. They cooperated with a medical device company to develop a unique surgical robot for spinal surgery, Orthobot, and experimented on porcine lumbar cones. The results of the study showed that the excellent rate of both radiation exposure time and pedicle screw implantation was higher than that of the traditional method and even superior to minimally invasive surgery in terms of incision. However, the experimental sample size was small, and it is not possible to determine for the time being whether other orthopedic conditions (e.g., osteoporosis) may affect the clinical results. Therefore, the generalizability of these results still requires further in-depth studies.

Li et al. [123] proposed a collaborative spinal robotic system to assist laminectomy in response to the lack of precision in a conventional decompressive laminectomy. The system's reliability was verified through experiments on porcine lumbar vertebrae and compared with the unarmed group. A comparison of the studies revealed that the time required, whether the vertebral plate was penetrated or not, and the remaining thickness of the vertebral plate was better than those of the freehand group in terms of lateral laminectomy in the machine group. The findings validate the safety of robot-assisted laminectomy. However, the efficiency and time of the system still need to be improved.

Derek et al. [124] used spinal robotics for the first time for pedicle screw placement in children, assessed the effectiveness of the procedure by recording intraoperative radiation vs. postoperative

screw position, and analyzed common causes of misalignment such as lateral deviation. The results show that even in pediatric patients, the technique can achieve results far exceeding freehand surgery. A detailed description of the above essential studies is shown in [Table 20](#).

**Table 20:** Relevant studies and their indicators

Source/Date	Type of assisted surgery	Surgical indicators	Dedicate	Limitations
[116]/2002	Total knee replacement	Tibiofemoral alignment actual vs. planned variance of only 0.8°.	Robot allows high-precision preoperative planning.	Increased operating time and cost.
[117]/2006	Total knee replacement	Surgical time of 104 min with a deviation of 0.65°.	Robotic assistance improves accuracy and consistency.	No long-term follow-up of patients.
[120]/2009	Posterior spinal surgery	The surgeon's fatigue and tremor were reduced.	Improved ergonomics and control.	Tested only on porcine spines.
[121]/2014	Spinal surgery	The screw accuracy was 98.5 percent and the time was 46.1 min with a radiation time of 1.3 s per screw.	Robotic assistance improves screw placement accuracy and reduces radiation exposure.	The large size of the 3D markers may lead to errors.
[122]/2020	Spinal surgery	The excellent rate of lumbar pedicle screw nailing channel was 96.7%.	Robotics ease the cost burden on patients.	The sample size of the experiment was too small.
[123]/2022	Spinal surgery	Operative time was 326 s and the incidence of complete plate penetration was 6.7% (30% with manual approach).	A new collaborative robotic system for laminectomy is proposed and the safety of the system is verified.	Does not integrate medical images with navigation and is therefore not suitable for clinical use.
[124]/2021	Spinal surgery	Accuracy was 98.7%, blood loss was 200 mL, and operative time was 235 min.	The first use of a robot in pediatric spine surgery.	CT scans were not used in some patients, so the accuracy of the experiment is biased.

### 3.2.5 Assisting Minimally Invasive Surgery

Numerous studies have shown that minimally invasive surgery is superior to open surgery in terms of safety and price [125]. Bowen et al. [126] applied a novel real-time image-guided robotic system for the first time to short-segment lumbar fusion surgery in patients with diagnostic degenerative diseases. By comparing the performance of the robot-assisted group and the unarmed group in terms of screw accuracy, discharge time, and bleeding found that the robotic group outperformed the unarmed group in all the metrics, and the study proved that the mechanical group had a lower economic cost. However, the data is too homogeneous and has yet to be applied in the clinic. Zhu et al. [127] used remote-controlled robot-assisted minimally invasive treatment of displaced femoral fractures, where the fracture reduction procedure was performed manually under teleoperation. The results proved that this robot-assisted system has high reduction accuracy, high safety, and low radiation exposure by setting up two trials as a control. With this application, precise fracture reduction can be achieved under visual control, opening the way for teleoperated robot-assisted minimally invasive surgery.

A detailed description of the above essential studies is shown in [Table 21](#).

**Table 21:** Relevant studies and their indicators

Source/Date	Type of assisted surgery	Surgical indicators	Dedicate	Limitations
[126]/2020	Short-segment lumbar fusion surgery	Intraoperative bleeding was 266.1 ml, and hospital recovery time was 1.8 days.	Better surgical metrics and better economics with robotic assistance.	Data sets are too homogenous and conclusions are not generalizable.
[127]/2017	Minimally invasive treatment of displaced femoral stem fractures	The mean errors for the axial and lateral views of the femur were 1.8 mm and 0.8 mm, respectively.	The robot-assisted system delivers better surgical outcomes and sets a precedent for teleoperated surgeries.	Failure to consider the effect of muscle contraction on surgery.

[Tables 19–21](#) summarize the use of different robotic technologies in various orthopedic surgeries. AI-based robots help to optimize the positioning of devices and tools, avoid the risk of exposure to healthcare workers, and overcome the difficulties of traditional techniques. With the help of these systems, implants are inserted into the patient at the correct angle and depth, improving the safety and accuracy of the procedure. Thus, using robotics in orthopedic surgeries will reduce the need for assistants, thus saving healthcare resources.

## 4 Discussion

### 4.1 Related Work

Federer et al. [128] provided a scoping review of the use of AI in orthopedics and its changing trends but needed to provide an in-depth study of its nature. Poduval et al. [129] provided a scientific discussion of using AI and machine learning in orthopedics but needed more specific classification studies. Lee et al. [130] classified orthopedic disorders but lacked explanations of the models.

Lalehzarian et al. [131] did a scientific discussion on the application of machine learning in orthopedic surgery, but it still needs to include the detection of images. Wang et al. [132] explained the advantages and disadvantages of AI in orthopedic clinical applications but did not include a scientific discussion of the specific applications. Cabitza et al. [6] classified the machine and deep learning models but lacked a discussion of the diseases. Kalmet et al. [133] did a scientific discussion of deep learning in fracture detection but needed a metrics analysis of the models. Therefore, the main contributions of this paper are as follows:

(1) This paper provides an in-depth metric analysis of deep learning and machine learning models. It systematically summarizes the relevant applications and their metrics, based on which scientific opinions on the future direction of improvement are provided.

(2) The classification of fractures and orthopedic diseases is discussed more comprehensively, and the advantages and shortcomings of AI in orthopedic image detection are summarised scientifically.

(3) The application of robotics in orthopedic surgery is explored, and the importance of robotics and the future direction of improvement are discussed rationally.

#### **4.2 Current Issues**

The core problem in the current healthcare field is that physician-centered healthcare resources cannot meet patients' needs, creating an urgent need for medical AI [134]. The above studies on fracture detection and disease diagnosis showed that the accuracy, specificity, and sensitivity of AI in image recognition are better than the independent judgment of physicians. In practical application, the collaborative diagnosis between AI and doctors can further shorten the manual diagnosis time, reduce the rate of leakage and misdiagnosis [135], accelerate the patients into the next step of treatment, and improve patient satisfaction. The application of AI robots in orthopedic surgery has significantly improved surgical safety, accuracy, and postoperative outcomes. Studies have shown that patients who underwent robotic-assisted surgery recovered faster after surgery and had superior physical indicators than patients who underwent unassisted surgery throughout [136–137]. This study confirms that robotic-assisted surgery saves medical resources and provides patients with better medical services. It shows that the application of AI in orthopedics has a good development prospect.

However, although most models studied perform well in metrics, AI is currently only used in a few clinical settings for assisted diagnosis. The main reason for this status quo is that more than just improving the indicators of the model is needed to promote the clinical use of AI. Some core potential and clinically useful indicators are often easily ignored by researchers, such as the model's ability to generalize, interpretability, etc., and the specific analysis of the current problems are as follows:

(1) It is difficult for researchers to obtain high-quality datasets. The quality and quantity of training datasets directly affect the model's performance. Still, getting large-scale patient data in the medical field is difficult due to relevant laws and regulations. In addition, the datasets usually need to be labeled with images by professional doctors, which is time-consuming, so the number of labeled datasets is limited. A decrease in the number of datasets can lead to a significant reduction in model accuracy. Therefore, the biggest challenge facing the current research is finding high-quality datasets and ways to overcome legal issues.

(2) Most models need better generalization ability in clinical practice. The main reasons for this problem are that only some models are externally validated, excellent metrics do not translate into good clinical performance, and most disease diagnostic studies usually focus on a single disease, which may be severely limited in practical applications.



(3) Although many scholars have contributed to promoting the application of AI in orthopedics, it is difficult to cover all orthopedic disease studies due to the wide variety of orthopedic diseases. As a result, AI cannot assist doctors in the clinic regarding rare orthopedic disorders.

(4) Models are not interpretable. Although the deep learning model performs well in accuracy, only some scholars have interpreted it. The algorithm's decision-making process uses opaque hidden layers, and the connections between inputs and outputs are unknown, resulting in the model producing predictions that are not scientifically interpretable. How the model learns from the training and test sets remains to be determined, which limits its use in clinical applications.

(5) Most studies have only dichotomized the disease, whereas a physician often needs to base his interpretation on multiple factors when diagnosing a patient's condition. Therefore, most studies have limitations in assisting physicians in clinical diagnosis.

(6) Surgical robots are expensive and have only a few auxiliary operating functions, so they do not realize economic benefits.

(7) Some studies have shown some contradictions between the robustness and accuracy of the models [138–139]. Most of the models proposed by researchers need to fully consider the relationship between robustness and precision, which leads to models that cannot be used stably in the clinic.

(8) The robotic system does not consider muscle tremors that may occur in patients during surgery, which may cause additional harm to the patient. In addition, it remains a controversial issue as to who will be held responsible if the model makes an error and causes damage to the patient.

### **4.3 Future Directions for Improvement**

Given the current clinical and technological problems, combined with the existing clinical experience and improvement methods, future research directions for the application of AI in orthopedics can be studied in the following aspects:

(1) For problems such as poor clinical effect of the model, the model's generalization ability can be improved by introducing a cross-validation step of validation set and test set in the model. At the same time, the attention mechanism and residual structure can be added to enhance the extraction and fusion of deep and shallow features by the model to maximize the preservation of the image's original information.

(2) For the problem of lack of dataset, researchers can adopt the migration learning approach to improve the convergence speed of the model. At the same time, it should actively cooperate with physicians to rationally communicate with patients and achieve accurate annotation with the assistance of physicians.

(3) To address the problem of model interpretability, the module responsible for interpretability can be considered trained together with the model, or the interpretability module can be added after the training is completed. Both methods can explain the judgment basis of the model to a certain extent.

(4) For situations like the robot's weak risk resistance during surgery, researchers should actively improve the algorithm and comprehensively consider possible intraoperative conditions to avoid accidents during surgery.

(5) For the function of the model, it is necessary to find a balance between considering robustness and accuracy so that the model is in pursuit of robustness and accuracy at the same time.

(6) Disease progression is a slow process, so when classifying the severity of the disease, it should be segmented as much as possible. Classifying the images used for training into multiple levels will help physicians in clinical practice.

## 5 Conclusions

In conclusion, this paper analyzes the studies related to AI in orthopedics, highlighting each study's contributions, strengths and weaknesses, and the directions that can be improved in the future. The rapid development of AI has enabled it to play an essential role in detecting orthopedic diseases and improving surgical indexes, effectively reducing the burden on doctors, optimizing the use of medical resources, and improving patient satisfaction. It is worth noting that the application of AI in orthopedics is not to replace professional physicians but to assist them in improving efficiency and diagnostic accuracy. It is foreseeable that in the future, the application of AI in orthopedics is expected to turn into a comprehensive diagnostic tool, with more machine learning and deep learning technologies being further developed and applied, based on which patients will enjoy more personalized, precise, minimally invasive, and remote services.

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