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Intelligent Deep Learning Based Multi-Retinal Disease Diagnosis and Classification Framework

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Abstract: In past decades, retinal diseases have become more common and affect people of all age grounds over the globe. For examining retinal eye disease, an artificial intelligence (AI) based multilabel classification model is needed for automated diagnosis. To analyze the retinal malady, the system proposes a multiclass and multi-label arrangement method. Therefore, the classification frameworks based on features are explicitly described by ophthalmologists under the application of domain knowledge, which tends to be time-consuming, vulnerable generalization ability, and unfeasible in massive datasets. Therefore, the automated diagnosis of multi-retinal diseases becomes essential, which can be solved by the deep learning (DL) models. With this motivation, this paper presents an intelligent deep learningbased multi-retinal disease diagnosis (IDL-MRDD) framework using fundus images. The proposed model aims to classify the color fundus images into different classes namely AMD, DR, Glaucoma, Hypertensive Retinopathy, Normal, Others, and Pathological Myopia. Besides, the artificial flora algorithm with Shannon's function (AFA-SF) based multi-level thresholding technique is employed for image segmentation and thereby the infected regions can be properly detected. In addition, SqueezeNet based feature extractor is employed to generate a collection of feature vectors. Finally, the stacked sparse Autoencoder (SSAE) model is applied as a classifier to distinguish the input images into distinct retinal diseases. The efficacy of the IDL-MRDD technique is carried out on a benchmark multi-retinal disease dataset, comprising data instances from different classes. The experimental values pointed out the



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superior outcome over the existing techniques with the maximum accuracy of 0.963.

Keywords: Multi-retinal disease; computer aided diagnosis; fundus images; deep learning; segmentation; intelligent models

1 Introduction

Retinal diseases are appeared as a common issue for aged people that degrades the power of the eyes, because of the blurred visualization and it results even in vision loss. The retina is one of the photosensitive layers, which is placed as a thin layer inside the eye. The retinal disease affects eye vision owing to blurred visualization and occasionally a whole vision loss [1]. The retina is affected by various infections like age-based molecular degeneration (AMD), diabetic retinopathy (DR), Diabetic Macular Edema (DME), Glaucoma, etc. The conventional eye disease diagnosis models are found to be a time-consuming task and require expert knowledge.

Macular diseases are the important causes of vision loss among elderly population and adults [2]. The macula, located at the central area of the retina, is accountable for central and sharp visions that let us view objects that are directly ahead. If the macular tissues become abnormally damaged or disordered, the lesions will appear. The numbers and types of lesions often determine the category and severity of eye diseases. For example, lesions, such as epiretinal membrane (ERM), edema, drusens, or cysts, are associated with various common diseases, e.g., age related macular degeneration and DR [3]. Therefore, detection and recognition of the retinal macular lesions are crucial for the clinical diagnosis and treatment of ophthalmopathy. It is predicted that around six hundred million people would have diabetes in 2040, with one-third anticipated to have DR, the major causes of blindness in working age adults around the world [4]. Mild NPDR is the earlier phase of DR, i.e., considered as the existence of microaneurysm. PDR is one of the innovative phases of DR and could lead to serious vision loss. Regular DR screening is significant thus appropriate treatment could be performed for preventing vision loss. Earlier phase interference through blood pressure and glycemia control could slow-down the development of DR and later phase intervention via intravitreal injection/photocoagulation could decrease vision loss. In Iceland and UK, systematic national DR screening has been conducted, DR is no longer the major cause of vision loss amongst working age adults. Even though routine DR screening is suggested with each research community, comprehensive DR screening is not extensively implemented, overcoming the problems associated with the accessibility of human assessors.

As subtle retinal lesions may not be obvious on ophthalmoscopy, retinal imaging technology has been rapidly developed during the past decades. Optical coherence tomography (OCT) is a noninvasive imaging technique, which utilizes infrared-light interferometry to image through the eye, aiming to see the structures beyond their surface. Recently, the advanced OCT technique can achieve a three-dimensional (3-D) tomography imaging of the eye with micrometer resolution, providing ophthalmologists the ability to visualize different types of lesions and thus assisting macular diagnosis and treatment. In the medical diagnoses, ophthalmologist frequently needs to automatically detect the presence of various macular cancers at all cross sections of the OCT volume. Such work is tedious, repetitive, and time consuming, which causes serious problems for the early detection and timely treatment of eye diseases. Therefore, development of automatic OCT image analysis techniques is an efficient way to provide supplemental information and support medical decisions for clinicians and ophthalmologists. In recent times, deep learning algorithm has assisted computer to learn from huge dataset in a manner which exceeds human abilities in various fields [5–7]. Many DL approaches using higher sensitivity and specificity were proposed for the detection/classification of specific disease conditions depending on medicinal images, involving retinal images. Present DL system for DR screening was mainly focused on the recognition of persons with vision threatening/DR referrable DR (worse/moderate NPDR) that implies the patient must be stated to ophthalmologist for closer follow-up/treatments [7]. But, the significance of detecting earlier phase DR should not be ignored. Evidence suggests that appropriate interference at an earlier phase to attain optimum controlling of blood pressure, lipid profiles, and glucose can considerably delay the development of DR and even reverse mild NPDR to DR free stages.

This paper presents an intelligent deep learning based multi-retinal disease diagnosis (IDL-MRDD) framework using fundus images. The proposed model aims to classify the color fundus images into different classes namely AMD, DR, Glaucoma, Hypertensive Retinopathy, Normal, Others, and Pathological_Myopia. In addition, the artificial flora algorithm with Shannon's function (AFA-SF) based multi-level thresholding technique is employed for image segmentation. Furthermore, SqueezeNet based feature extractor is employed to generate a collection of feature vectors. Lastly, the stacked sparse Autoencoder (SSAE) model is used for the classification of multi-retinal diseases. A wide range of simulations is performed to point out the enhanced performance of the IDL-MRDD technique on a benchmark multi-retinal disease dataset, comprising data instances from different classes.

2 Related Works

In Karthikeyan et al. [8], DCNN based ML method was employed to detect the 12 main retinal problems from the minimum set of fundus images. Further, the method has been cross-validated using real time fundus images. The method is established to be dominant in its ability, specificity, and efficacy for minimizing misclassification. Fauw et al. [9] employed a new DL framework to clinical heterogeneous sets of 3D optical coherence tomography scans from a patient refer to the main eye hospital. They determine efficiency in creating a suggestion which exceeds/reaches that of experts on a range of sight threatening retinal diseases afterward training over 14,884 scans. Mihalov et al. [10] presented a DL method based software framework for retinal disease diagnoses. The multiclass disease classifications are depending on CNN trained by an OCT B scan image. The TL and Data augmentation is utilized for overcoming few requirements and limitations of DL use in ophthalmology. The DL classifications are incorporated in a software platform i.e., usable, easily available, secure, and reliable.

Jain et al. [11] intended to manually categorize images using retinal problems from this healthier on without implementing any feature extraction/explicit segmentation. Instead, they utilize a DL method for manually classifying any retinal fundus image as diseased/healthy. The framework of the networks is fast and simple. The method was verified on 2 datasets, involving real person retinal fundus images attained from nearby hospitals. Rajagopalan et al. [12] proposed a DCNN architecture for the classification and diagnosis of Average, DME, and DMD efficiently. Firstly, despeckling of the input OCT image is executed by the Kuan filters for removing inherent speckle noise. Furthermore, the CNN networks are tuned with hyper-parameter optimization methods. Moreover, K-fold validations are performed to guarantee full use of the datasets. Arunkumar et al. [13] introduced the retina based disease diagnoses with DL method based FE approach. This method assists in emerging automatic screening systems, i.e., able to diagnose retina for the diseases like DR, age related molecular degeneration, retinoblastoma, macular bunker, retinitis pigmentosa, and retinal detachment. Few diseases share a standard feature that makes the classification complex. For overcoming the aforementioned problems, DL-FE and multiclass SVM classifiers are employed.

Li et al. [14] presented a new self-supervised feature learning approach by efficiently using multimodal data for retinal disease diagnoses. For this purpose, initially, synthesize the respective FFA modal and later create a person feature based softmax embedding objective. The objectives learn person similarity feature and modality invariant feature. Using this method, the NN captures the semantically distributed data through distinct modals and the obvious visual similarities among the persons. This approach is tested on 2 public standard data sets for retinal disease diagnoses. Yoo et al. [15] exhibit that FSL with a GAN approach could enhance the applicability of the DL method in OCT diagnoses of uncommon diseases. The 4 main groups with a huge amount of datasets and 5 uncommon diseases classes with FSL datasets are involved in this work. Beforehand training the classifiers, they created GAN model for generating pathological OCT images of all uncommon diseases from average OCT images. The Inception-v3 framework has been trained by increased training datasets, and the last method was authenticated by a separate test data set. Yan et al. [16] examined the segmentation of thin and thick vessels individually by suggesting a 3 phase DL method. The vessel segmentation tasks are separated into 3 phases, such as thin vessel segmentation, vessel fusion, and thick vessel segmentation. Since, better discriminative features can be learned to split segmentation of thin vessels and thick vessels, this method reduces the negative impact created by their high imbalanced ratio. The last vessel fusion phase improves the result by additionally detecting non-vessel pixels and improve the entire vessel thickness reliability.

3 The Proposed IDL-MRDD Model

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In this study, a new multi-retinal disease diagnosis model using IDL-MRDD technique is presented to determine different types of retinal diseases. The IDL-MRDD technique method involves pre-processing in three stages such as image resizing, noise removal, and contrast improvement. Fig. 1 illustrates the overall block diagram of IDL-MRDD model. The detailed working of these processes is given in the succeeding sections.

3.1 Design of AFA-SF Based Segmentation Technique

At this stage, the preprocessed retinal fundus images are applied as input to the AFA-SF technique. Entropy is generally adapted for computing the uncertainty of a parameter [17]. The process is given below: Select an image frame of size M^*N . Next, the gray values of pixel using coordinate (x, y) could be given by (x, y), for $x \in \{1, 2, M\}$ and $y \in \{1, 2, N\}$. Where L represent the amounts of gray level of image I_0 and the sets of each gray level $\{0, 1, 2, \dots, L-1\}$ could be represented by G:

$$f(x, y) \in G \forall (x, y) \in image$$

(1)

The standardized histogram of the image could be denoted by $H = \{h_0, h_1, \dots, h_{L-1}\}$.

For multi-thresholding problems, the aforementioned formula could be given by;

$$H(T) = h_0(t_1) + h_1(t_2), \dots, h_{L-1}(t_{k-1})$$
⁽²⁾

$$T* = \max_{\mathrm{T}} \left\{ H\left(T\right) \right\} \tag{3}$$

where T * denotes the optimum threshold and can be optimally chosen using AFA to generate effective segmentation output.



Figure 1: Block diagram of IDL-MRDD model

The AFA is a state-of-art SI based optimization method presented by Cheng et al. [18] and it can be depending upon flora migration and reproduction procedure. It is established on six standard operations and demonstrates powerful exploration capability with fast convergences. In this method, the original plant is generated primarily and the scattered seed, are known as off-spring plants, with a specific distance. Initially, the early population is created arbitrarily with *N* original plant.

$$X_{ij} = r \times D \times 2 - D \tag{4}$$

Whereas the original plant position is represented as $X_{i,j}$, *i* and *j* denote dimensional and numbers of plants, correspondingly, also *r* indicates uniform distribution from range of [0,1]. Then, the propagate distance D_j is evaluated to all the plants. The evaluation of propagation distance of plant is based on prior 2 generations.

$$D_j = D_{1j} \times r \times c_1 + D_{2j} \times r \times c_2 \tag{5}$$

where propagation distances of grandparent and parent plants denote D_{2j} and D_{1j} , correspondingly, c_1 and c_2 denotes learning coefficient, and r indicates uniform distribution. The novel grandparent propagation is given as:

$$D'_{1j} = D_{2j}$$
 (6)

The novel parent spreading distance is given as follows:

$$D'_{2j} = \sqrt{\frac{\sum_{i=1}^{N} \left(X_{ij} - X'_{ij}\right)^2}{N}}$$
(7)

The off-spring plant locations near the original plant are estimated as:

$$X'_{ij\times m} = R_{ij\times m} + X_{ij} \tag{8}$$

where X'_{ij} represent off-spring plant locations, *m* indicates amount of off-spring is created with single plant, and $R_{i,j \times m}$ denotes normal distribution arbitrary amount by mean zeroand variance D_j . Few

created off-spring would survive and others wonot, either off-spring is alive/not can be defined by the likelihood of surviving which is estimated utilizing proportion based selection.

$$p = \left| \sqrt{\frac{F\left(X'_{ij \times m}\right)}{F_{\max}}} \right| \times Q^{(j \times m - 1)}$$
(9)

where the chosen likelihood is represented as $Q^{(j \times m-1)}$ and its value is among zero and one, F_{\max} represents maximum fitness of overall off-spring, and every single off-spring plant denote $F(X'_{i,j \times m})$. The off-spring would survive when the likelihood of surviving p is higher compared to r, in which r denotes uniform distribution arbitrary amount in the interval zero and one. The N off-spring plant is chosen by survived off-spring as novel original plant for succeeding iteration. The AF method is repeated till it encounters the end condition. At last, an optimum solution is selected.

Algorithm 1: Pseudo-code of AFA

Initiation: Produce N original plant arbitrarily by Eq. (4); calculate fitness of every individual; select an optimum solution When t < MaxIter do for *i* from 1 to N * M do Evaluate the proportion distance by Eqs. (5)–(7)Create off-spring plant by Eq. (8)if p > r then Off-spring plant live else Off-spring plant not alive end if end for Calculate novel solution Arbitrarily select N novel original plant The novel solution replace the older one when the value is optimum end while return an optimum solutions

3.2 SSAE Based Image Classification

During image classification, the feature vectors are fed into the SSAE model to allot proper class labels to it. Related to SAE, training an SSAE includes detecting an optimum parameter $\theta = (W, b_h, b_x)$ simultaneously by minimalizing the discrepancies among reconstruction and input. When the optimum parameter is θ attained, the SSAE yield a function: $R^{d_x} \rightarrow R^{d_{h(2)}}$ which transform input pixel intensity of image patches to a novel feature representation $h^{(2)} = f(x) \in R^{d_{h(2)}}$ of nuclear structure. Fig. 2 depicts the overall structure of the SSAE.

In SSAE model, every training patch x(k) of pixel intensity is denoted as a higher-level structure depiction of non-nuclei/nuclei patch $h^{(2)}(k)$ in the 2nd hidden layer of the method. Each training patch could be given by $\{h^{(2)}(k), y(k)\}_{k=1}^{N}$ whereas for every $k \in \{1, 2, ..., N\}$, $\{h^{(2)}(k), y(k)\}$ denote a pair of higher-level features and its labels. For the 2 class classification problems deliberated in this study, the labels of k th patch represent $y(k) \in \{0, 1\}$, whereas zero and one represents the non-nuclear and nuclear patches, correspondingly. Assume that in the SSAE learning process, the label data Y is not employed. Hence, SSAE learning is an unsupervised learning system [19,20]. When the higher-level

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features learning process are completed, the learned higher-level depiction of nuclear structure, and its labels $\{h^{(2)}(k), y(k)\}_{k=1}^N$, fed into the output layer, i.e., softmax classifier. It is a supervised method that generalizes LR as

$$f_{W^{(3)}}(z) = \frac{1}{1 + \exp(-W(3)^{T_{Z}})}$$
(10)

whereas $f_{W(3)}(.)$ denotes a sigmoid function using parameters $W^{(3)}$. if the input z of SMC denotes a higher-level depiction of nuclear structure learned using SSAE, the SMC parameters $W^{(3)}$ is trained by training set $\{h^{(2)}(k), y(k)\}_{k=1}^{N}$ for minimizing the objective functions. By minimalizing the objective functions regarding $W^{(3)}$ through the gradient descent dependent method, parameters $W^{(3)}$ could be defined.



Figure 2: Framework of SSAE

4 Performance Validation

This section examines the performance of the IDL-MRDD technique against a benchmark dataset [21], which consists of 200 images under AMD class, 200 images under DR class, 200 images under Glaucoma class, 92 images under Hypertensive_Retinopathy (HR), 200 images under Normal, 200 images under Others, and 200 images under Pathological Myopia. Few sample test images are provided in Fig. 3. The size of images is 1444×1444 and 2304×1728 .

Fig. 4 shows the confusion matrices generated by the IDL-MRDD technique on the classification of multi-retinal diseases with distinct training/testing sizes. On the applied training/testing sizes of 60:40, the IDL-MRDD technique has classified the AMD, DR, Glaucoma, HR, Normal, Others, and PM into 133, 194, 124, 88, 197, 200, and 155 respectively. Besides, on the applied training/testing sizes of 70:30, the IDL-MRDD approach has classified the AMD, DR, Glaucoma, HR, Normal, Others, and PM into 145, 196, 138, 92, 197, 200, and 153 correspondingly. Additionally, on the applied training/testing sizes of 80:20, the IDL-MRDD method has classified the AMD, DR, Glaucoma, HR, Normal, Others, and PM into 155, 198, 150, 92, 197, 200, and 164 correspondingly.



Figure 3: Sample images



Figure 4: Confusion matrix analysis of IDL-MRDD model

Tab. 1 provides the overall classification results of the IDL-MRDD technique under distinct classes and training/testing sizes. The table values denoted that the IDL-MRDD technique has resulted in effective classification outcomes on all the applied classes. For instance, with training/testing size of 60:40, the IDL-MRDD technique has classified the AMD, DR, Glaucoma, HR, Normal, Others, and PM by obtaining an accuracy of 0.944, 0.993, 0.938, 0.962, 0.962, 0.948, and 0.942 respectively. In the meantime, with training/testing size of 70:30, the IDL-MRDD manner has classified the AMD, DR, Glaucoma, HR, Normal, Others, and PM by attaining an accuracy of 0.954, 0.995, 0.952, 0.964, 0.973, 0.957, and 0.940 correspondingly. Likewise, with training/testing size of 80:20, the IDL-MRDD methodology has classified the AMD, DR, Glaucoma, HR, Normal, Others, and PM by reaching an accuracy of 0.964, 0.996, 0.961, 0.972, 0.982, 0.965, and 0.949 correspondingly.

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No. of classes	Accuracy	Precision	Recall	F-score
Training/Testing (60:40)				
Age_Related_Macular_Degeneration	0.944	0.957	0.665	0.785
Diabetic_Retinopathy	0.993	0.985	0.970	0.977
Glaucoma	0.938	0.969	0.620	0.756
Hypertensive_Retinopathy	0.962	0.662	0.957	0.782
Normal	0.962	0.811	0.985	0.889
Others	0.948	0.749	1.000	0.857
Pathological_Myopia	0.942	0.838	0.775	0.805
Training/Testing (70:30)				
Age_Related_Macular_Degeneration	0.954	0.973	0.725	0.831
Diabetic_Retinopathy	0.995	0.985	0.980	0.983
Glaucoma	0.952	1.000	0.690	0.817
Hypertensive_Retinopathy	0.964	0.662	1.000	0.797
Normal	0.973	0.860	0.985	0.918
Others	0.957	0.784	1.000	0.879
Pathological_Myopia	0.940	0.836	0.765	0.799
Training/Testing (80:20)				
Age_Related_Macular_Degeneration	0.964	0.987	0.775	0.868
Diabetic_Retinopathy	0.996	0.985	0.990	0.988
Glaucoma	0.961	1.000	0.750	0.857
Hypertensive_Retinopathy	0.972	0.719	1.000	0.836
Normal	0.982	0.908	0.985	0.945
Others	0.965	0.816	1.000	0.899
Pathological_Myopia	0.949	0.845	0.820	0.833

Table 1: Classification results analysis of IDL-MRDD technique under varying training/testing sizes

Tab. 2 depicts the average results analysis of the IDL-MRDD technique under different training/testing sizes. The table values demonstrated that the IDL-MRDD technique has gained enhanced performance under all training/testing sizes. For instance, with the training/testing size of 60:40, the IDL-MRDD technique has attained an increased accuracy of 0.956, precision of 0.853, recall of 0.853, and F-score of 0.836. Meanwhile, with the training/testing size of 70:30, the IDL-MRDD manner has reached an improved accuracy of 0.962, precision of 0.872, recall of 0.878, and F-score of 0.860. Eventually, with the training/testing size of 80:20, the IDL-MRDD algorithm has gained a maximum accuracy of 0.970, precision of 0.894, recall of 0.903, and F-score of 0.889.

Training/Testing size	Accura	cy Precisio	on Recall	F-score
Training/Testing (60:40)	0.956	0.853	0.853	0.836
Training/Testing (70:30)	0.962	0.872	0.878	0.860
Training/Testing (80:20)	0.970	0.894	0.903	0.889
Average	0.963	0.873	0.878	0.862

 Table 2: Average results analysis of IDL-MRDD technique

Fig. 5 showcases the ROC analysis of the IDL-MRDD technique under varying training/testing sizes. The figure demonstrated that the IDL-MRDD technique has resulted in a maximum ROC of 98.1826, 99.1630, and 99.6356 under the training/testing size of 60:40, 70:30, and 80:20 respectively. An extensive comparative study of the IDL-MRDD with existing techniques takes place in Tab. 3.







Figure 5: ROC analysis of IDL-MRDD model with different training/testing sizes

Methods	Accuracy	Precision	Recall	F1-score
IDL-MRDD	0.963	0.873	0.878	0.862
CNN-DL	0.809	0.812	0.805	0.810
MLP	0.815	0.821	0.813	0.818
RBF	0.831	0.839	0.830	0.832
SVM	0.815	0.821	0.814	0.817
ANN	0.750	0.759	0.749	0.751
NB	0.669	0.672	0.783	0.747

 Table 3: Comparative analysis of IDL-MRDD model with existing techniques

Fig. 6 investigates the performance of the IDL-MRDD technique with existing techniques interms of accuracy. The figure reported that the ANN and NB models have shown poor outcomes with the lower accuracy of 0.750 and 0.669. Additionally, the CNN-DL, MLP, and SVM techniques have showcased slightly improved accuracy values of 0.809, 0.815, and 0.815 respectively. Moreover, the RBF technique has demonstrated competitive performance with an accuracy of 0.831. However, the proposed IDL-MRDD technique has accomplished superior performance with higher accuracy of 0.963.

Fig. 7 examines the performance of the IDL-MRDD approach with recent methods with respect to precision. The figure stated that the NB and ANN methods have demonstrated worse results with the lesser precision of 0.672 and 0.759. Also, the CNN-DL, MLP, and SVM manners have demonstrated somewhat increased precision values of 0.812, 0.821, and 0.821 correspondingly. Furthermore, the RBF method has demonstrated competitive performance with a precision of 0.839. However, the proposed IDL-MRDD technique has accomplished superior performance with a maximum precision of 0.873.



Figure 6: Comparative analysis of IDL-MRDD model in terms of accuracy



Figure 7: Comparative analysis of IDL-MRDD model in terms of precision

Fig. 8 inspects the performance of the IDL-MRDD technique with existing manners interms of recall. The figure described that the ANN and NB models have shown poor outcomes with the lower recall of 0.749 and 0.783. Likewise, the CNN-DL, MLP, and SVM manners have showcased slightly improved recall values of 0.805, 0.813, and 0.814 respectively. Besides, the RBF technique has exhibited competitive performance with the recall of 0.830. But, the presented IDL-MRDD methodology has accomplished higher performance with a maximum recall of 0.878.

Fig. 9 showcases the performance of the IDL-MRDD method with existing algorithms interms of F1-score. The figure clear that the NB and ANN models have outperformed least outcome with the lower F1-score of 0.747 and 0.751. At the same time, the CNN-DL, SVM, and MLP techniques have depicted slightly enhanced F1-score values of 0.810, 0.817, and 0.818 correspondingly. Moreover, the RBF technique has demonstrated competitive performance with an F1-score of 0.832. Eventually, the projected IDL-MRDD method has accomplished maximum performance with an increased F1-score of 0.862. By looking into the above-mentioned tables and figures, it is obvious that the IDL-MRDD

technique has accomplished effectual outcome over the other existing techniques and it can be used as an appropriate tool for multi-retinal disease diagnosis using retinal fundus images.



Figure 8: Comparative analysis of IDL-MRDD model in terms of recall



Figure 9: Comparative analysis of IDL-MRDD model in terms of F1-score

5 Conclusion

In this study, a new multi-retinal disease diagnosis model using IDL-MRDD technique is presented to determine different types of retinal diseases. The proposed IDL-MRDD model involves different stages of operation such as preprocessing, AFA-SF based segmentation, SqueezeNet based feature extraction, and SSAE based image classification. The design of AFA to optimally select the threshold values for multi-level thresholding helps to improve the overall segmentation outcomes. A wide range of simulations is performed to point out the enhanced performance of the IDL-MRDD technique on a benchmark multi-retinal disease dataset, comprising data instances from different classes. The experimental values pointed out the superior outcome over the existing techniques. As

a part of future extension, advanced DL models can be employed as the segmentation techniques and thereby boost the diagnostic outcomes. Besides, hybrid metaheuristic algorithms can be designed for the hyperparameter tuning of the DL based feature extractors.

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