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Novel Apodized Fiber Bragg Grating Applied for Medical Sensors: Performance Investigation

Ramya Arumugam¹, Ramamoorthy Kumar^{1,*}, Samiappan Dhanalakshmi¹, Khin Wee Lai², Lei Jiao^{3,*} and Xiang Wu⁴

¹Department of Electronics and Communication Engineering, College of Engineering and Technology, SRM Institute of Science and Technology, Kattankulathur, Chengalpattu, 603203, India

²Department of Biomedical Engineering, Faculty of Engineering, Universiti Malaya, Kuala Lumpur, 50603, Malaysia

³General Hospital of Xuzhou Mining Group, Xuzhou, 221000, China

⁴School of Medical Information & Engineering, Xuzhou Medical University, Xuzhou, 221000, China

*Corresponding Authors: Ramamoorthy Kumar. Email: kumarr@srmist.edu.in; Lei Jiao. Email: jiaolei515@xzhmu.edu.cn

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ABSTRACT

Sensors play an important role in shaping and monitoring human health. Exploration of methods to use Fiber Bragg Grating (FBG) with enhanced sensitivity has attracted great interest in the field of medical research. In this paper, a novel apodization function is proposed and performance evaluation and optimization of the same have been made. A comparison was conducted between various existing apodization functions and the proposed one based on optical characteristics and sensor parameters. The results evince the implementation of the proposed apodization function for vital sign measurement. The optical characteristics considered for evaluation are Peak Resonance Reflectivity level, Side Lobes Reflectivity level and Full Width Half Maximum (FWHM). The proposed novel apodization novel function has better FWHM, which is narrower than the FWHM of uniform FBG. Sensor characteristics like a quality parameter, detection accuracy and sensitivity also show improvement. The proposed novel apodization function is demonstrated to have a better shift in wavelength in terms of temperature and pulse measurement than the existing functions. The sensitivity of the proposed apodized function is enhanced with a Poly-dimethylsiloxane coating of varying thickness, which is 6 times and 5.14 times greater than uniform Fiber Bragg grating and FBG with the proposed novel apodization function, respectively, enhancing its utilization in the field of medicine.

KEYWORDS

Fiber bragg grating; apodization; optical sensing; temperature; strain; sensitivity

1 Introduction

Fiber Bragg Gratings (FBGs) is a fiber with a core refractive index induced with periodic variation in the direction of the fiber axis for a length called grating length. A specific wavelength is reflected back due to this periodic grating and it is known as Bragg wavelength (λ_B). The periodicity (Λ), modulation of the index (Δn) and length (L) of the grating determines and manages the optical



properties of FBG [1–4]. The advantages of these grating-based sensors are their resistance to EMI. lightweight, robustness, compact size, stability, remote sensing ability, easy fabrication, installation and maintenance [5,6]. This enables their implementation in various areas of the optical field such as structural health monitoring, medical applications, measurement of temperature and strain in aerospace, as lasers, as buffers, as filters, as multiplexers [7-12], heat transfer application [13] and sewer corrosion [14]. Uniform FBG has a main lobe corresponding to Bragg wavelength in addition to the presence of many side lobes. The occurrence of these side lobes affects the peak resonance detection, making it undesirable characteristics for sensing applications. Apodization is the technique that can be applied to reduce or eliminate these side lobes. Various articles [15-23] suggested implementing the existing functions or proposed novel apodization functions for the improvement of sensing characteristics, strain and temperature measurement, dispersion compensation, structural health monitoring, etc. In a few literatures, sensitivity enhancement has been achieved by using coating materials [24,25]. In the earlier stage, metals and their compounds having high thermal expansion coefficients, were used to amplify temperature sensitivity [26-29]. Due to the complex fabrication process and residual stress, this method was not widely applicable. Later, the utilization of polymer with high thermal expansion and thermo optic coefficient has been researched to enhance the sensitivity. Various works on different polymers such as polydimethylsiloxane, polyvinyl alcohol, polycarbonate, polymethylmethacrylate and polystyrene have been reported [30-43]. The variant of grating, known as Bragg Fibers, is implemented to enhance sensing applications [44-46]. The light propagated in the cladding region is measured for sensing the measure. The application of artificial intelligence improves the performance of the sensor in health care which makes it a promising future in sensor technology [47–49]. In this work, a novel apodization function is proposed to enhance the sensing characteristics and to maximize the usage of FBG as a vital sign sensor, which measures pulse as strain and temperature. Enhancement in wavelength shift in the sensing signal is also measured. Improvement in sensitivity is reported using polydimethylsiloxane coating. Table 1 shows the comparison between the existing and the proposed apodization functions for various applications.

Reference	Existing apodization	Proposed apodization	Application
[15]	Uniform, Blackman, Nutall, Gaussian, Hamming, Sinc	$g(z) = 0.55 + 0.45 * \cos(2\Pi/L)$	Dispersion compensation
[16]	Uniform, Gaussian, Blackman, Sine, Tanh Types I & II, Cauchy, Barthan Welch, Cones	$g(z) = \left[J_0\left\{\cos\left(\frac{3x}{L}\right)\right\}\right]^8 \left[\cos\left(\frac{\Pi z}{L+5}\right)\right]$	Sensing application
[17]	Sine, Hamming, Tanh, Bartlett, Blackman, Sinc, Gaussian, Cauchy, Raised sine	-	Sensing application

Table 1: Comparison of existing and proposed work

(Continued)

Table 1 (continued)						
Reference	Existing apodization	Proposed apodization	Application			
[18]	Uniform, Raised sine, Sinc, Gaussian, Nutall	-	Temperature measurement in DWDM systems.			
[19]	Gaussian, Tanh4z	$g(\mathbf{x}) = J_0 \left[\cos\left(\frac{3z}{L}\right) \right]^8 \left[\cos\left(\frac{2z}{L} - 1\right) \right]^4$	Structural health Monitoring			
[21]	Sinc, Gaussian, Raised cosine	-	-			
Proposed	Uniform, Gaussian, Barthan, Sine, Welch, Cones, Hamming, Blackman, Nutall, Bessel	$g(\mathbf{x}) = \left\{ 1 - \left[\left(\mathbf{x} - \frac{L}{2} \right)^2 / \left(\frac{L}{2} \right)^2 \right] \right\}^4$	Medical sensing applications			

The organization of the present work is as follows: Section 2 gives the principle of operation and the coupled mode theory of uniform FBG, the functions of various existing apodization profiles and properties of coating materials considered for the proposed apodization function. Section 3 deals with the results and discussion. Section 4 summarizes the conclusion, followed by references.

2 Theoretical Background

2.1 Principle of Uniform Fiber Bragg Grating (UFBG)

The refractive index variation of the Fiber Bragg Grating with periodic variation along its axis is given as

$$n(z) = n_{core} + \Delta n \cos\left(\frac{2\pi z}{\Lambda}\right)$$
(1)

where n_{core} is the refractive index of the core region, z is the direction of propagation, A is the grating periodicity, Δn is the refractive index modulation. Bragg wavelength (λ_B), is given as

$$\lambda_{\rm B} = 2n_{\rm eff}\Lambda \tag{2}$$

where n_{eff} is the core effective refractive index. Using couple mode theory, the reflectivity of uniform grating FBG is given as

$$\mathbf{R} (\mathbf{L}, \lambda_{\mathrm{B}}) = \frac{k^2 \sinh^2 (sL)}{\Delta \beta^2 \sinh^2 (sL) + s^2 \cosh^2 (sL)}$$
(3)

304

where k is the coefficient of coupling, $\Delta\beta$ is the detuning wave vector and is given as $\beta \cdot (\Pi/\Lambda)$ and $s^2 = k^2 - \beta^2$. k, the coupling coefficient is represented as

$$k = \frac{\pi \,\Delta n}{\lambda} M p \tag{4}$$

where Mp is part of the power contained in fiber core. β is the propagation constant and given as $2\pi n_{core}/\lambda$. At centre wavelength, maximum reflectivity happens as $\Delta\beta = 0$.

$$\mathbf{R}_{\max}\left(\mathbf{L},\lambda_{\mathrm{B}}\right) = \tanh^{2}(kL) \tag{5}$$

The strain-based shift in Bragg wavelength is given as

$$\Delta\lambda_{\rm B} = \lambda_{\rm B} \left(1 - p_{\rm e}\right) \Delta\varepsilon \tag{6}$$

$$p_{e} = n_{eff}^{2} \left[p_{11} - v_{f} \left(p_{11} + p_{12} \right) \right] / 2 \tag{7}$$

where p_e is the effective photoelastic coefficient, n_{eff} is the effective refractive index and v_f is the Poisson ratio. p_{11} and p_{12} are Pockel's piezo coefficients for strain optic tensor. For silica, $p_{11} = 0.121$, $p_{12} = 0.27$ and $v_f = 0.17$.

The wavelength shift due to the change in temperature is given as

$$\Delta\lambda_{\rm B} = \lambda_{\rm B} \left(\alpha_{\rm f} + \alpha_{\rm n}\right) \Delta T \tag{8}$$

where $\alpha_{\rm f}$ is thermal expansion coefficient and $\alpha_{\rm n}$ is thermo optic coefficient and its corresponding values are $5.5 \times 10^{-7} \frac{1}{k}$ and $8.3 \times 10^{-6} \frac{1}{k}s$, respectively. The sensitivity of bragg wavelength for both temperature and strain can be represented as

$$\Delta\lambda_{\rm B} = \lambda_{\rm B} \left[(1 - p_{\rm e}) \,\Delta\varepsilon + (\alpha_{\rm f} + \alpha_{\rm n}) \,\Delta T \right] \tag{9}$$

Fig. 1 shows the diagrammatic representation of the working of FBG.



Figure 1: Theory of FBG

2.2 Coupled Mode Theory

The propagation of electromagnetic waves inside the fiber core can be represented using coupled mode theory (CMT). The electric field distribution in forward and backward propagating waves can be defined by equations as shown below, respectively.

$$E_{a}(z,t) = A(z) e^{i(\omega t - \beta z)}$$
(10)

$$\mathbf{E}_{\mathbf{b}}\left(\mathbf{z},\mathbf{t}\right) = \mathbf{B}\left(\mathbf{z}\right)\mathbf{e}^{\mathbf{i}\left(\omega\mathbf{t}+\beta\mathbf{z}\right)} \tag{11}$$

. .

where A(z) and B(z) are complex amplitudes and are described as

$$\frac{dA(z)}{dz} = ikB(z) e^{-2i\Delta\beta z}$$

$$\frac{dB(z)}{dB(z)} = ikB(z) e^{2i\Delta\beta z}$$
(12)

$$\frac{dz}{dz} = -ik^* A(z) e^{2i\Delta\beta z}$$
(13)

For $0 \le z \le L$. By applying boundary conditions B(0) = Bo and A(L) = AL and solving for closed form solutions,

$$a(z) = A(z) e^{-i\beta z}$$
(14)

$$\mathbf{b}\left(\mathbf{z}\right) = \mathbf{B}\left(\mathbf{z}\right)\mathbf{e}^{\mathbf{i}\boldsymbol{\beta}\mathbf{z}} \tag{15}$$

Scattering matrix is used to express the reflected and transmitted wave as

$$\begin{bmatrix} a \ (0) \\ b \ (L) \end{bmatrix} = \begin{bmatrix} S11 & S12 \\ S21 & S22 \end{bmatrix} \begin{bmatrix} a \ (L) \\ b \ (0) \end{bmatrix}$$
(16)

Substituting values of a(0) and b(L) from Eqs. (14) and (15) results in

$$S11 = S22 = \frac{iSe^{-i\beta 0L}}{-\Delta\beta \sinh(SL) + iScosh(SL)}$$
(17)

$$S12 = \frac{k}{k^*} S21e^{2i\beta 0L} = \frac{k\sinh(SL)}{-\Delta\beta\sinh(SL) + iS\cosh(SL)}$$
(18)

To obtain the general solution of coupled mode equation, an effective method known as the Transfer matrix method (T-matrix) has been used, in which a single grating is subdivided into a series of separate gratings (N) of uniform type and described aa s square 2 * 2 matrix. This provides greater flexibility and the precision is based on the number of sections, N. The T-matrix is described as

$$\begin{bmatrix} a (0) \\ b (0) \end{bmatrix} = \begin{bmatrix} T11 & T12 \\ T21 & T22 \end{bmatrix} \begin{bmatrix} a (L) \\ b (L) \end{bmatrix}$$
(19)

where,

$$T11 = T^* 22 = \frac{\Delta\beta \sinh(SL) + iS\cosh(SL)}{iS} e^{-i\beta 0L}$$
(20)

$$T12 = T^* 21 = \frac{ksinh\left(SL\right)}{iS} e^{-i\beta 0L}$$
(21)

The reflectivity of FBG is expressed as

$$\mathbf{R} = \left| \frac{T21}{T11} \right|^2 \tag{22}$$

2.3 Existing Apodization Functions

The apodization functions considered for comparison of performance evaluation are listed in this section. Apodization functions are chosen from the literature [15-21].

1. Uniform

$$g(x) = 1 \text{ for } 0 \le x \le L \tag{23}$$

2. Gaussian

$$g(x) = \exp\left(-\ln 2\left(\frac{2(x-\left(\frac{L}{2}\right)}{0.5L}\right)^2\right) \quad \text{for } 0 \le x \le L$$
(24)

3. Barthan

$$g(x) = 0.62 - 0.48 \left(\frac{x}{L} - 0.5\right) + 0.38 \cos\left(\frac{x}{L} - 0.5\right) \quad \text{for } 0 \le x \le L$$
(25)

4. Sine

$$g(x) = \sin\left(\frac{\pi x}{L}\right) \quad \text{for } 0 \le x \le L$$
 (26)

5. Welch

$$g(\mathbf{x}) = 1 - \left[\left(\mathbf{x} - \frac{L}{2} \right)^2 / \left(\frac{L}{2} \right)^2 \right] \quad \text{for } 0 \le \mathbf{x} \le \mathbf{L}$$
(27)

6. Cones

$$g(\mathbf{x}) = \left\{ 1 - \left[\left(\mathbf{x} - \frac{L}{2} \right)^2 / \left(\frac{L}{2} \right)^2 \right] \right\}_2 \quad \text{for } 0 \le \mathbf{x} \le \mathbf{L}$$
(28)

7. Hamming

$$g(x) = 0.54 - 0.46 \cos\left(\frac{2\pi x}{L}\right) \quad \text{for } 0 \le x \le L$$
 (29)

8. Blackman

$$g(x) = 0.42 - 0.5 \cos\left(\frac{2\pi x}{L}\right) + 0.08 \cos\left(\frac{4\pi x}{L}\right) \quad \text{for } 0 \le x \le L$$
 (30)

9. Nutall

$$g(x) = 0.3635819 - 0.48917755 \left(\frac{2\pi x}{L}\right) + 0.1365996 \left(\frac{4\pi x}{L}\right) - 0.0106411 \left(\frac{6\pi x}{L}\right)$$

for $0 \le x \le L$ (31)

10. Bessel [17]

$$g(x) = J_0 \left[\cos\left(\frac{3x}{L}\right) \right]^8 \left[\cos\left(\frac{2x}{L} - 1\right) \right]^4 \text{ for } 0 \le x \le L$$
(32)

 J_0 -Bessel function of the first kind of zero order and L is the grating length.

2.4 Proposed Apodization Function

In this work, we propose a new apodization function for better sensor characteristics and reflectivity level. The above mentioned characteristics can be attained by using a compact transform which results in narrow bandwidth with high resolution. The strategy to make a transform compact is to increase the power of the exponent or multiply with the increasing functions. The former one is implemented to optimize the apodization function, maximizing its usage as a sensor. The proposed

306

CMES, 2023, vol.135, no.1

apodization function is given in Eq. (33).

$$g(\mathbf{x}) = \left\{ 1 - \left[\left(\mathbf{x} - \frac{L}{2} \right)^2 \middle/ \left(\frac{L}{2} \right)^2 \right] \right\}^4 \quad \text{for } 0 \le \mathbf{x} \le \mathbf{L}$$
(33)

where L is the grating length. The performance of the existing and proposed apodization functions can be analyzed based on side lobe reflectivity level (MSL), sensitivity, side lobe suppression ratio (SLSR), quality parameter and detection accuracy [16].

$$Sensitivity = \frac{Change in peak resonance reflectivity}{change in refractive index}$$
(34)

Detection Accuracy =
$$\frac{Resonance \ peak \ wavelenth}{FWHM}$$
 (35)

Quality Parameter =
$$\frac{Sensitivity}{FWHM}$$
 (36)

The schematic representation of the proposed novel apodized FBG based sensor system is shown in Fig. 2. It embodies source, FBG based sensor, circulator, data acquisition system and Optical interrogator. FBG interrogator and PC are used to measure the reflected signal to determine the measurand. The measurement of applied temperature and strain are given as a shift in peak wavelength.



Figure 2: Schematic diagram of sensing system

2.5 Optical Characteristics of Coating Materials

The coating on uniform FBG enhances its sensitivity. The schematic diagram of UFBG with coating is shown in Fig. 3. Polymer based materials such as Poly-dimethylsiloxane (PDMS), Poly-carbonate (PC) and Polymethyl methacrylate (PMMA) have been considered for coating on FBG to enhance sensitivity. These polymers are safe on human skin and can be used directly for non-invasive measurements using FBG on human beings. These materials also have good mechanical and temperature stability. The optical properties of these materials are given in Table 2. Though all materials are safe on human skin, due to its high thermal expansion and thermo optic coefficient, PDMS is considered and performance is analyzed in enhancing the sensitivity of the proposed

apodization function. The advantages of PDMS are its low cost, high thermal stability, low electrical conductivity, transparency in optical characteristics, high durability and oxidative stability, less toxicity and biocompatibility [41–43]. Sylgard 184 type of PDMS is regarded for analysis.



Figure 3: Schematic diagram of UFBG with coating

Polymer	Refractive index	Thermo-optic coefficient (/°C)	Thermal expansion coefficient (/°C)	Poisson's ratio	Reference
PDMS	1.399	-4.5×10^{-4}	3×10^{-4}	0.4950	[41]
PC	1.585	-0.9×10^{-4}	$1.7 imes 10^{-4}$	0.3182	[39]
PMMA	1.48	-1.3×10^{-4}	2.2×10^{-4}	0.34	[39]

Table 2: Optical characteristics of different polymers

3 Results and Discussion

Using Opti-Grating software, simulations to investigate the optical properties of various existing apodization functions with the proposed apodization function are evaluated by considering a single mode fiber (silica) with 1.46 as refractive index of core and 1.45 as refractive index of cladding. The center wavelength of 1550 nm is considered. The length of the grating has been varied from 1 mm to 15 mm and index depth is varied from 1×10^{-4} to 2.5×10^{-4} for performance evaluation. Fig. 4 exhibits the profile of all the existing apodizations studied and the proposed novel apodization function. Compared to other existing functions, the proposed apodization provides better truncation at both the ends of the grating length which effectively reduces the side lobe levels and narrows the bandwidth.



Figure 4: (Continued)



Figure 4: (Continued)



Figure 4: (Continued)



Figure 4: (Continued)



Figure 4: Profile of various apodizations (a) Uniform (b) Gaussian (c) Barthan (d) Sine (e) Welch (f) Cones (g) Hamming (h) Blackman (i) Nutall (j) Bessel (k) Proposed

An increase in the reflectivity level of the main lobe, for varying grating length with $\Delta n = 0.0001$ and index modulation with grating length 10 mm, is shown in Figs. 5a and 5b. In uniform FBG, peak resonance level increases by 99.5% and 96.54%, respectively, for increasing index change and grating length. The proposed apodization function shows 88.4% and 98.28% increase in reflectivity level of peak resonance for increasing index change and grating length, respectively.



Figure 5: Mainlobe reflectivity level for existing and proposed Apodization for (a) Varying Grating length (b) Varying Index Change

Figs. 6a shows the increasing reflectivity level of the left side lobe and 6b shows the reflectivity of the right-side lobe for increasing modulation index. Figs. 7a and 7b show the reflectivity of the left and right-side lobes for increasing grating length. The non-linearity in the side lobe reflectivity level is due to the mismatch between the scattered light and the spacing of the high refractive zone.



Figure 6: Reflectivity level for increasing modulation index (a) Left-side lobe (b) Right-side lobe



Figure 7: Reflectivity level for increasing grating length (a) Left-side lobe (b) Right-side lobe

In cones apodization function, left and right-side lobe levels increase by 22.84% and 22.43%, respectively, for increasing index change and by 63.02% and 71.04%, respectively, for increasing grating length. Likewise, for Gaussian function, left and right-side lobe level increases by 29.67% and 22.04%, respectively, for increasing index change and by 59.19% and 66.55% respectively for increasing grating length. The proposed apodization function shows 22.39% and 22.92% increase in the left and right-side lobe reflectivity levels, respectively, for increasing index modulation and 68.15% and 74.56% increase in left and right-side lobe reflectivity levels respectively for increasing grating length.

Table 3 shows the optical properties of various apodization profiles. The Least FWHM of **0.06 nm** is given by Gaussian, Hamming and Blackman apodizations. Better detection accuracy is obtained by narrow FWHM. The second lowest FWHM of **0.07 nm** is achieved by the proposed apodization function, which is **41.67%** lesser than the FWHM of UFBG. The proposed novel apodized function has a side lobe level of $-34.6852 \, dB$ which is nearer to Gaussian and shows **148%** reduction compared to UFBG. A side lobe suppression ratio of $-30.3563 \, dB$ which is **71.16%** more compared to UFBG has been attained by the proposed apodization function.

Apodization types	Reflectivity (dB)	MSL (dB)	SLSR (dB)	FWHM (nm)	Slope (dB/nm)
Uniform	-0.5648	-14.0133	-17.7356	0.12	-125.8200
Gaussian	-2.9001	-35.4861	-32.5860	0.06	-67.4465
Barthan	-0.5952	-14.3129	-13.7177	0.12	-115.8685
Sine	-1.9503	-29.6796	-27.7293	0.12	373.9926
Welch	-1.7587	-28.7008	-26.9421	0.12	225.6871
Cones	-2.7796	-34.9280	-32.1484	0.12	140.8413
Hamming	-2.7266	-35.2340	-32.5074	0.06	20.3894
Blackman	-4.1295	-34.7823	-30.6528	0.06	-43.2555
Nutall	-4.0572	-16.8327	-12.7755	0.12	86.1890
Bessel	-2.3881	-34.9419	-32.5538	0.12	186.9966
Proposed	-4.3289	-34.6852	-30.3563	0.07	-51.8398

Table 3: Apodization profiles: Optical properties

Table 4 shows evaluation parameters considered for the comparison of existing and proposed apodization function. The proposed novel apodization results in a greater sensitivity of **5.9083 AU/RIU** and the Uniform apodization has lower sensitivity (**1.6783 AU/RIU**). The sensitivity of the proposed apodization function increases by **3.52 times**, compared to UFBG. The proposed novel apodization function has a detection accuracy of **22383** which is **71.42%** more compared to UFBG. The Blackman apodization has the peak quality parameter of **96.5067 AU/nm-RIU**. The quality parameter of **84.4043 AU/nm-RIU** has been achieved by the proposed system which makes it **503%** more than UFBG. Evaluations have been carried out for $\Delta n = 0.0001$ and L = 10 mm. The comparison between the UFBG and the proposed apodization function is tabulated in Table 5.

Type of apodization	FWHM (nm)	Sensitivity (AU/RIU)	Detection accuracy	Quality parameter (AU/nm- RIU)	Wavelength shift($\Delta \lambda_{\rm B}$)/ $\mu \varepsilon$	Wavelength shift $(\Delta \lambda_{\rm B})/^{\circ}{\rm C}$
Uniform	0.12	1.6783	13057	13.9858	1.2pm	12pm
Gaussian	0.06	4.8888	26114	81.4667	1.2pm	12pm
Barthan	0.12	1.7450	13057	14.5418	1.2pm	12pm
Sine	0.12	3.9112	13057	32.5933	1.2pm	12pm
Welch	0.12	3.6736	13057	30.6133	1.2pm	12pm
Cones	0.12	4.7757	13057	39.7975	1.2pm	12pm
Hamming	0.06	4.7309	26114	78.8483	1.2pm	12pm
Blackman	0.06	5.7904	26114	96.5067	1.2pm	12pm
Nutall	0.12	5.7316	13057	47.7633	1.2pm	12pm
Bessel	0.12	4.4017	13057	36.6808	1.2pm	12pm
Proposed	0.07	5.9083	22383	84.4043	1.4pm	14pm

 Table 4: Apodization profiles: performance evaluation

Table 5: Comparison between UFBG and the proposed apodization function

Parameter	Uniform FBG	Proposed apodization	Comments (%)
FWHM (nm)	0.12	0.07	↓41.67
MSL (dB)	-14.0133	-34.6852	↑148
SLSR (dB)	-17.7356	-30.3563	↑71.16
Sensitivity (AU/RIU)	1.6783	5.9083	↑252
Quality parameter (AU/nm-RIU)	13.9858	84.4043	↑503
Detection accuracy	13057	22383	↑71.42

Induced periodic refractive index modulation along the fiber core is given as

$$\Delta n(z) = \Delta n_0 \left(1 + f(z) v \cos \left[\frac{2\Pi z}{\Lambda} + \varphi(z) \right] \right)$$
(37)

where f(z) is apodization profile function, v is fringe visibility of index change, $\varphi(z)$ is grating chirp and Δn_0 is the averaged index change. Eq. (37) explains the dependence of effective modulation on the apodization profile. This dependence is responsible for the shift in the wavelength, as Bragg shift depends on the effective refractive index from Eq. (2). The proposed novel apodization function has an increased wavelength shift for the applied temperature and strain based on this. Wavelength shift for the strain applied is shown in Fig. 8a. The strain was applied in steps of 50 $\mu\varepsilon$. The proposed novel apodization function achieves a shift of **1.4 pm/\mu\varepsilon**. Change in Bragg wavelength relating to varying temperature (steps of 10°C) is shown in Fig. 8b. The proposed apodization function achieves a wavelength shift of **14 pm/°C** (Table 4).



Figure 8: Shift in wavelength for (a) Variation in strain (b) Variation in temperature

Optimization of grating length (L) and index modulation (Δn) is essential to determine the maximum reflectivity of peak resonance. To achieve 100% reflectivity, a proper selection of 'L' and ' Δn ' should be made. In this study, simulation was performed for various values of index modulation and the grating length and observations are tabulated as shown in Table 6. Fig. 9 shows the graphical representation of Table 6. Reflectivity level of the left and right-side lobes for various index modulations and grating lengths, are shown in Fig. 10. The optimized values are calculated as L = 15 mm and $\Delta n = 0.00025$, in which the reflectivity level of peak resonance is 100% and the reflectivity level of the left and right-side lobes are -23.5077 dB and -23.5921 dB, for the proposed apodization function.

Grating length (mm)	Reflectivity of main lobe (d)
	$\Delta n = 0.0001$	$\Delta n = 0.00015$	$\Delta n = 0.0002$	$\Delta n = 0.00025$
5	-127.3710	-123.9490	-4.2684	-2.9585
10	-4.3289	-2.0968	-1.0252	-0.5018
15	-2.1575	-0.7402	-0.2534	-0.0866
20	-1.1044	-0.2648	-0.0631	-0.0150
25	-0.5734	-0.0950	-0.0158	-0.0026
30	-0.3004	-0.0345	-0.0039	0
35	-0.1584	-0.0125	0	0
40	-0.0839	-0.0045	0	0
45	-0.0447	-0.0017	0	0
50	-0.0239	0	0	0

Table 6: Optimization for the proposed function for various index modulations and grating lengths



Figure 9: Main lobe reflectivity vs. index modulation and grating length

Sensitivity enhancement with PDMS coating for varying thickness is shown in Fig. 11. The temperature sensitivity is 72 pm/°C, which is 5.14 times higher than that of the proposed apodized FBG without coating and 6 times higher than UFBG without coating. The negative thermal expansion coefficient develops a blue shift in the wavelength for increasing temperatures. There exists a non-linearity in the wavelength shift from 50°C-70°C based on the thickness of the PDMS coating. As the present study focuses on the temperature measurement of human beings, the coating thickness does not show any effect on temperature sensitivity. Strain sensitivity does not show any change and is linear with increasing strain. The wavelength shift is $1.2 \text{ pm/}\mu\epsilon$ and shows a red shift.



Figure 10: Side lobe reflectivity vs. Index modulation and grating length (a) Left-side lobe (b) Rightside lobe



Figure 11: Sensitivity variation for different coating thickness of PDMS (a) Varying temperature (b) Varying strain

4 Conclusion

Apodization functions are implemented to enhance the performance of sensors by suppressing side lobes and making FHWM narrower. The proposed novel apodization is manifested to have suitable performance parameters to implement it as a sensor in the field of medicine. Narrow FWHM, highest sensitivity (3.52 times more compared to UFBG) and detection accuracy (71.42% more than UFBG), make it a preferable solution for sensing employment. Enhancement in sensitivity as 1.4 pm/ μ e and 14 pm/°C is shown by the proposed novel apodization for strain and temperature measurement respectively. With optimization, maximum reflectivity of 100% has been achieved for

15 mm of grating length and index modulation of 0.00025 for the proposed apodization function. Enhancement in temperature sensitivity of 72 pm/°C was achieved by using PDMS coating, which is 5.14 times greater than the proposed apodization without coating, enabling its implementation for monitoring vital signals in human beings.

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References

- 1. Kashyap, R. (2010). Fiber bragg gratings. Elsevier, USA, Academic Press.
- Yu, Q., Zhang, Y., Dong, Y., Li, Y. P., Wang, C. et al. (2012). Study on optical fiber bragg grating temperature sensors for human body temperature monitoring. 2012 Symposium on Photonics and Optoelectronics, pp. 1–4. Shanghai, China, IEEE.
- 3. Liu, L., Zhang, H., Zhao, Q., Liu, Y., Li, F. (2007). Temperature-independent FBG pressure sensor with high sensitivity. *Optical Fiber Technology*, 13(1), 78–80. DOI 10.1016/j.yofte.2006.09.001.
- 4. Campanella, C. E., Cuccovillo, A., Campanella, C., Yurt, A., Passaro, V. M. (2018). Fibre bragg grating based strain sensors: Review of technology and applications. *Sensors*, *18*(9), 3115. DOI 10.3390/s18093115.
- 5. Othonos, A., Kalli, K. (2000). Fiber bragg gratings: Fundamentals and applications in telecommunications and sensing. *Physics Today*, *53*(*5*), *61*. DOI 10.1063/1.883086.
- 6. Nicolas, M. J., Sullivan, R. W., Richards, W. L. (2016). Large scale applications using FBG sensors: Determination of in-flight loads and shape of a composite aircraft wing. *Aerospace*, 3(3), 18. DOI 10.3390/aerospace3030018.
- Lecourt, J. B., Duterte, C., Narbonneau, F., Kinet, D., Hernandez, Y. et al. (2012). All-normal dispersion, all-fibered PM laser mode-locked by SESAM. *Optics Express*, 20(11), 11918–11923. DOI 10.1364/OE.20.011918.
- Keshk, M. M., Ashry, I. A., Aly, M. H., Okaz, A. M. (2007). Analysis of different fiber bragg gratings for use in a multi-wavelength erbium doped fiber laser. 2007 National Radio Science Conference, pp. 1–13. Cairo, Egypt, IEEE.
- 9. Ashry, I., Shalaby, H. M. (2010). All-optical variable delay buffer for next generation optical networks. 2010 12th International Conference on Transparent Optical Networks, pp. 1–3. Munich, Germany, IEEE.
- 10. Ashry, I., Shalaby, H. M. (2010). Tunable fabry-perot interferometer based on fiber bragg gratings. 2010 17th International Conference on Telecommunications, pp. 534–537. Doha, Qatar, IEEE.
- 11. Orr, P., Niewczas, P. (2011). High-speed, solid state, interferometric interrogator and multiplexer for fiber bragg grating sensors. *Journal of Lightwave Technology*, 29(22), 3387–3392. DOI 10.1109/JLT.2011.2169044.
- 12. Goncalves, A. F., Ferreira, L. A., Araujo, F. M. M., Mendes, P. M., Correia, J. H. (2010). A smart skin PVC foil based on FBG sensors for monitoring strain and temperature. *IEEE Transactions on Industrial Electronics*, 58(7), 2728–2735. DOI 10.1109/TIE.2010.2057233.

- Chakravartula, V., Rakshit, S., Dhanalakshmi, S., Kumar, R., Narayanamoorthi, R. (2021). Linear temperature distribution sensor using FBG in liquids—Local heat transfer examination application. *IEEE Sensors Journal*, 21(15), 16651–16658. DOI 10.1109/JSEN.2021.3078731.
- 14. Raju, B., Kumar, R., Dhanalakshmi, S., Dooly, G., Duraibabu, D. B. (2021). Review of fiber optical sensors and its importance in sewer corrosion factor analysis. *Chemosensors*, 9(6), 118. DOI 10.3390/chemosensors9060118.
- Adel Naguib, B., Maher Ata, M., Alzalabani, M. M., Yousif, B. B. (2021). Performance evaluation and enhancement of apodized fiber bragg grating for dispersion compensation. *AIP Advances*, 11, 015231. DOI 10.1063/5.0026190.
- 16. Maiti, S., Singh, V. (2020). Performance analysis of apodized fiber bragg gratings for sensing applications. *Silicon, 14,* 1–7.
- 17. Ashry, I., Elrashidi, A., Mahros, A., Alhaddad, M., Elleithy, K. (2014), April). Investigating the performance of apodized fiber bragg gratings for sensing applications. *Proceedings of the 2014 Zone 1 Conference of the American Society for Engineering Education*, pp. 1–5. Indianapolis, Indiana, USA, IEEE.
- Mohammed, N. A., Ali, T. A., Aly, M. H. (2014). Evaluation and performance enhancement for accurate FBG temperature sensor measurement with different apodization profiles in single and quasidistributed DWDM systems. *Optics and Lasers in Engineering*, 55, 22–34. DOI 10.1016/j.optlaseng.2013.10.013.
- 19. Dwivedi, K. M., Trivedi, G., Khijwania, S. K. (2020). Theoretical study and optimization of apodized fiber bragg grating for single and quasi-distributed structural health monitoring applications. 2020 30th International Conference Radioelektronika (RADIOELEKTRONIKA), pp. 1–6. Bratislava, Slovakia, IEEE.
- 20. Ashik T, J., Kachare, N., Kumar, D. S. (2017). Analysis of simultaneous measurement of temperature and strain using different combinations of FBG. *LET THERE BE LIGHT: Reflections of a Congress on Light*, 1849(1), 020031.
- 21. Ugale, S., Mishra, V. (2010). Fiber bragg grating modeling, characterization and optimization with different index profiles. *International Journal of Engineering Science and Technology*, 2(9), 4463–4468.
- 22. Jiang, S. C., Wang, J., Sui, Q. M., Ye, Q. L., Wang, L. J. (2015). Study of three-component FBG vibration sensor for simultaneous measurement of vibration, temperature, and verticality. *Journal of Sensors, 38,* 2865.
- 23. Arumugam, R., Kumar, R., Dhanalakshmi, S. (2022). Optimization and performance evaluation of apodization function for fiber bragg grating as vital sign sensor. *Kuala Lumpur International Conference on Biomedical Engineering*, pp. 341–350. Springer, Cham.
- 24. Chakravartula, V., Samiappan, D., Kumar, R. (2020). Sensitivity enhancement analysis due to different coating materials of fibre bragg grating-based depth sensor for underwater applications. *Optical and Quantum Electronics*, 52 (1), 1–15. DOI 10.1007/s11082-019-2144-x.
- Samiappan, D., Kesarikiran, A. V. S., Chakravartula, V. (2020). Enhancing sensitivity of fiber bragg gratingbased temperature sensors through teflon coating. *Wireless Personal Communications*, 110(2), 593–604. DOI 10.1007/s11277-019-06744-w.
- 26. Gupta, S., Mizunami, T., Yamao, T., Shimomura, T. (1996). Fiber bragg grating cryogenic temperature sensors. *Applied Optics*, 35(25), 5202–5205. DOI 10.1364/AO.35.005202.
- Lupi, C., Felli, F., Ippoliti, L., Caponero, M. A., Ciotti, M. et al. (2005). Metal coating for enhancing the sensitivity of fibre bragg grating sensors at cryogenic temperature. *Smart Materials and Structures*, 14(6), N71–N76. DOI 10.1088/0964-1726/14/6/N02.
- 28. Jung, J., Nam, H., Lee, B., Byun, J. O., Kim, N. S. (1999). Fiber bragg grating temperature sensor with controllable sensitivity. *Applied Optics*, *38*(*13*), 2752–2754. DOI 10.1364/AO.38.002752.
- 29. Lin, G. C., Wang, L., Yang, C. C., Shin, M. C., Chuang, T. J. (1998). Thermal performance of metal-clad fiber bragg grating sensor. *IEEE Photonics Technology Letters*, 10(3), 406–408. DOI 10.1109/68.661425.

- 30. Rong, Q., Sun, H., Qiao, X., Zhang, J., Hu, M. et al. (2012). A miniature fiber—Optic temperature sensor based on a fabry–Perot interferometer. *Journal of Optics*, 14(4), 045002. DOI 10.1088/2040-8978/14/4/045002.
- Sampath, U., Kim, D., Kim, H., Song, M. (2018). Cryogenic temperature sensor based on fresnel reflection from a polymer-coated facet of optical fiber. *IEEE Sensor Journal*, 18(9), 3640–3644. DOI 10.1109/JSEN.2018.2813303.
- 32. Romano, I. H., Hernández, D. M., Hernández, C. M., Hernandez, D. M., Villatoro, J. (2015). Highly sensitive temperature sensor based on a polymer-coated microfiber interferometer. *IEEE Photonics Technology Letters*, 27(24), 2591–2594. DOI 10.1109/LPT.2015.2478790.
- 33. Estella, J., Vicente, P. D., Echeverria, J. C., Garrido, J. J. (2010). A Fibre-optic humidity sensor based on a porous silica xerogel film as the sensing element. *Sensors and Actuators B*, 149(1), 122–128. DOI 10.1016/j.snb.2010.06.012.
- 34. Zhang, Y., Wang, F., Liu, Z., Duan, Z., Cui, W. et al. (2017). Fiber-optic anemometer based on singlewalled carbon nanotube coated tilted fiber bragg grating. *Optics Express*, 25(2), 24521–24530. DOI 10.1364/OE.25.024521.
- 35. Wong, W. C., Chan, C. C., Chen, L. H., Li, T., Lee, K. X. et al. (2012). Polyvinyl alcohol coated photonic crystal optical fiber sensor for humidity measurement. *Sensors and Actuators B*, 174, 563–569. DOI 10.1016/j.snb.2012.07.032.
- 36. Muto, S., Suzuki, O., Amano, T., Morisawa, M. A. (2003). Plastic optical fibre sensor for real-time humidity monitoring. *Measurement Science and Technology*, *14*(6), 746–750. DOI 10.1088/0957-0233/14/6/306.
- 37. Salunkhe, T. T., Choi, H. W., Park, S. J., Kim, J. H., Kim, I. T. (2020). High sensitivity temperature sensor based on fresnel reflection with thermosensitive polymer: Control of morphology and coating thickness. *Japanese Journal of Applied Physics, 59*, SGGG06. DOI 10.7567/1347-4065/ab5c7d.
- 38. El-Amassi, D. M., Taya1, S. A., Vigneswaran, D. (2018). Temperature sensor utilizing a ternary photonic crystal with a polymer layer sandwiched between Si and SiO₂ layers. *Journal of Theoretical and Applied Physics*, *12(4)*, 293–298. DOI 10.1007/s40094-018-0308-x.
- 39. Esposito, F., Zotti, A., Palumbo, G., Zuppolini, S., Consales, M. et al. (2018). Liquefied petroleum gas monitoring system based on polystyrene coated long period grating. *Sensors*, 18(5), 1435. DOI 10.3390/s18051435.
- 40. Zhang, Z., Zhao, P., Lin, P., Sun, F. (2006). Thermo-optic coefficients of polymers for optical waveguide applications. *Polymer*, 47(14), 4893–4896. DOI 10.1016/j.polymer.2006.05.035.
- 41. Fendinger, N. J. (2000). Polydimethylsiloxane (PDMS): Environmental fate and effects. In: *Organosilicon chemistry IV: From molecules to materials*, pp. 626–638. DOI 10.1002/9783527619917.
- 42. Turek, I., Tarjanyi, N., Martincek, I., Kacik, D. (2014). Effect of mechanical stress on optical properties of polydimethylsiloxane. *Optical Materials*, *36*(*5*), 965–970. DOI 10.1016/j.optmat.2013.12.049.
- 43. Nedoma, J., Fajkus, M., Vasinek, V. (2016). Influence of PDMS encapsulation on the sensitivity and frequency range of fiber-optic interferometer. *Optical Materials and Biomaterials in Security and Defence Systems Technology XIII*, pp. 99940P.1–99940P.7. SPIE.
- 44. Arumugam, R., Ramamoorthy, K., Samiappan, D. (2021). Study of various structures of bragg fibers based on modal analysis. *ICOL-2019*, pp. 271–274. Springer, Singapore.
- 45. Yeh, P., Yariv, A. (1978). Theory of bragg fiber. *Journal of Optical Society of America*, 68(9), 1196–1201. DOI 10.1364/JOSA.68.001196.
- 46. Guo, S., Albin, S., Rogowski, R. S. (2004). Comparative analysis of bragg fibers. *Optics Express, 12(1),* 198–207. DOI 10.1364/OPEX.12.000198.

- 47. Teo, K., Yong, C. W., Muhamad, F., Mohafez, H., Hasikin, K. et al. (2021). The promise for reducing healthcare cost with predictive model: An analysis with quantized evaluation metric on readmission. *Journal of Healthcare Engineering*, 2021. DOI 10.1155/2021/9208138.
- Yeoh, P. S. Q., Lai, K. W., Goh, S. L., Hasikin, K., Hum, Y. C. et al. (2021). Emergence of deep learning in knee osteoarthritis diagnosis. *Computational Intelligence and Neuroscience*, 2021. DOI 10.1155/2021/4931437.
- 49. Miotto, R., Wang, F., Wang, S., Jiang, X., Dudley, J. T. (2018). Deep learning for healthcare: Review, opportunities and challenges. *Briefings in Bioinformatics*, 19(6), 1236–1246. DOI 10.1093/bib/bbx044.